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Journal article

**Architectural changes of the biceps femoris long head after concentric or eccentric training**

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1 **Title:**

2 Architectural changes of the biceps femoris after concentric or eccentric training.

3

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21 Adaptability of biceps femoris architecture

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24

25 **ABSTRACT**

26 **Purpose:** To determine i) the architectural adaptations of the biceps femoris long head (BFIf)  
27 following concentric or eccentric strength training interventions; ii) the time course of  
28 adaptation during training and detraining. **Methods:** Participants in this randomized  
29 controlled trial (control [n=28], concentric training group [n=14], eccentric training group  
30 [n=14], males) completed a 4-week control period, followed by 6 weeks of either concentric-  
31 or eccentric-only knee flexor training on an isokinetic dynamometer and finished with 28  
32 days of detraining. Architectural characteristics of BFIf were assessed at rest and during  
33 graded isometric contractions utilizing two-dimensional ultrasonography at 28 days pre-  
34 baseline, baseline, days 14, 21 and 42 of the intervention and then again following 28 days of  
35 detraining. **Results:** BFIf fascicle length was significantly longer in the eccentric training  
36 group ( $p < 0.05$ ,  $d$  range: 2.65 to 2.98) and shorter in the concentric training group ( $p < 0.05$ ,  $d$   
37 range: -1.62 to -0.96) after 42 days of training compared to baseline at all isometric  
38 contraction intensities. Following the 28-day detraining period, BFIf fascicle length was  
39 significantly reduced in the eccentric training group at all contraction intensities compared to  
40 the end of the intervention ( $p < 0.05$ ,  $d$  range: -1.73 to -1.55). There was no significant change  
41 in fascicle length of the concentric training group following the detraining period.  
42 **Conclusions:** These results provide evidence that short term resistance training can lead to  
43 architectural alterations in the BFIf. In addition, the eccentric training-induced lengthening of  
44 BFIf fascicle length was reversed and returned to baseline values following 28 days of  
45 detraining. The contraction mode specific adaptations in this study may have implications for  
46 injury prevention and rehabilitation.

47 **Key Words:** fascicle; muscle adaptation; hamstring; ultrasound; randomized controlled trial

## 48 INTRODUCTION

49 The ability of a muscle to produce force is partly governed by its architectural characteristics,  
50 such as muscle thickness, pennation angle and fascicle length (17). Architectural  
51 characteristics have been shown, in many different muscles, to change when exposed to  
52 mechanical stimuli, such as resistance training (2, 3, 21, 28, 32). Understanding the changes  
53 to muscle architecture in response to a given stimulus is important when aiming to alter  
54 muscle function and the risk of injury (2, 3, 7, 36).

55 During the terminal swing phase of the gait cycle, the hamstrings are required to actively  
56 lengthen to decelerate the extending knee and flexing hip (38). It is during this phase of the  
57 gait cycle where the hamstrings are at their longest, with the biceps femoris long head (BF<sub>lh</sub>)  
58 reaching approximately 110% of its length during upright stance (35). These high force,  
59 lengthening actions of the hamstrings may contribute to the high rate of strain injuries during  
60 running (26), the majority of which occur in the BF<sub>lh</sub> (16, 24). Interestingly, a previously  
61 strain injured BF<sub>lh</sub> possesses shorter fascicle lengths and greater pennation angles when  
62 compared to the contralateral uninjured BF<sub>lh</sub> (36). Furthermore differences in fascicle length  
63 can alter function, with muscles that possess longer fascicles having a greater maximal  
64 shortening velocity when compared to those with shorter fascicles (6, 17). Therefore it is  
65 important to develop an understanding of how muscle architecture can be altered by physical  
66 training in order to influence function, as well as guide hamstring strain injury prevention and  
67 rehabilitation practices.

68 Despite the large amount of research showing a range of architectural adaptations following  
69 eccentric training interventions (2, 3, 31), investigations which outline the time course for  
70 adaptation, including a period of detraining, are limited. Furthermore, the previous research  
71 into the adaptability of the BF<sub>lh</sub> following a training intervention only compared eccentric

72 training to a non-training control group (28). It is therefore it is unclear how BFlf  
73 architectural adaptations might differ after eccentric and concentric strength training.

74 Given the high incidence of hamstring injury in the BFlf (16, 24), it is of interest to see how  
75 its architecture is altered following either concentric or eccentric strength training. Therefore  
76 the purposes of this study were to: 1) determine the architectural adaptations of the BFlf  
77 following either a concentric or eccentric strength training intervention and; 2) determine the  
78 time course of BFlf architectural adaptations during a 6-week training intervention, and  
79 following a 28 day period of detraining.

## 80 **METHODS**

### 81 **Participants**

82 Twenty-eight recreationally active males (age  $22.3 \pm 4.2$  y; height  $1.81 \pm 0.07$  m; body mass  
83  $76.9 \pm 8.2$  kg) with no history of lower limb injury in the past 12 months were recruited to  
84 participate in this study. All participants provided written informed consent prior to testing  
85 and training which was undertaken at the Australian Catholic University, Fitzroy, Victoria,  
86 Australia. Ethical approval for the study was granted by the Australian Catholic University  
87 Human Research Ethics Committee.

### 88 **Study design**

89 Participants undertook a maximal isokinetic dynamometry familiarization session no less  
90 than 7 days prior to having their BFlf architecture assessed. The familiarization session and  
91 architectural assessment was completed on both limbs. Following this initial testing session  
92 (*28 days pre-baseline*), the participants were paired according to passive BFlf fascicle length  
93 and randomly assigned to one of two training groups (allocation ratio 1:1) to undertake either  
94 concentric- or eccentric-only knee flexor strength training. All participants (n=28) returned to  
95 the lab 4 weeks later (*baseline*) and had the maximal knee flexor strength and BFlf

96 architectural characteristics assessed on both limbs. Following this the participants underwent  
97 6 weeks of either a concentric- or eccentric–strength training intervention in a randomly  
98 selected limb (the contralateral limb served as a within-participant control). BFlf architecture  
99 of both limbs was re-assessed at days 14, 21 and 42 of the intervention, as well as 28 days  
100 after the completion of the strength training intervention. Knee flexor strength of both limbs  
101 was re-tested at the end of the training intervention (*day 42*) and 28 days after the completion  
102 of the intervention. All tests were performed at the same time of the day for each participant.

### 103 **Outcome measures**

#### 104 **Isokinetic dynamometry**

105 All knee flexor strength testing was completed on a Humac Norm® isokinetic dynamometer  
106 (CSMI, Massachusetts, U.S.A), on both legs (left or right) in a randomized order. Participants  
107 were seated on the dynamometer with their hips flexed at approximately 85° from neutral and  
108 were restrained by straps around the tested/exercised thigh, waist and chest to minimise  
109 compensatory movements. All seating variables (e.g. seat height, pad position, etc.) were  
110 recorded to ensure the replication of the participants' positions. Gravity correction for limb  
111 weight was also conducted and range of motion was set between 0° and 90° of knee flexion  
112 (full extension = 0°) with the starting position for each contraction during strength testing  
113 being 90° of knee flexion. The starting position for all training contractions were dependent  
114 on training group, with the concentric training group starting from 0° of knee extension and  
115 the eccentric group beginning from 90°. Prior to all testing sessions, participants undertook a  
116 warm-up consisting of three sets of three concentric knee extension and flexion contractions  
117 at an angular velocity of 240°/s. The intensity of these contractions increased each set (1<sup>st</sup> set  
118 ~75% and 2<sup>nd</sup> set ~90% of the participants perceived maximum) until the final set at this  
119 velocity was performed at a maximal level. The test protocol began one minute following the  
120 final warm-up set and consisted of three sets of three repetitions of concentric and eccentric

121 maximal voluntary contractions of knee flexion at 60°/s and 180°/s (30s inter-set rest). For all  
122 concentric knee flexion efforts, the participants were instructed to ‘pull down’ against the  
123 lever as fast as possible, whereas during eccentric contractions they were told to ‘resist’ the  
124 lever arm from extending their knee as hard as they could. All participants were provided  
125 visual feedback of their efforts as well as being verbally encouraged by the investigators to  
126 ensure maximal effort for all contractions. The testing order of contraction modes was  
127 randomized across the participant pool and the testing protocol has been previously reported  
128 to not alter concentric- or eccentric-knee flexor strength (37). Dynamometer torque and lever  
129 position data were transferred to computer at 1 kHz and stored for later analysis where it was  
130 fourth-order low pass Butterworth filtered (5 Hz). Peak torques at 240, 180 and 60°/s for  
131 concentric and 180 and 60°/s for eccentric knee flexion were defined as the mean of the six  
132 highest torque values for each contraction mode at each velocity.

### 133 **BFlf architectural assessment**

134 Muscle thickness and pennation angle of the BFlf were determined from ultrasound images  
135 taken along the longitudinal axis (Figure 1) of the muscle belly utilizing a two dimensional,  
136 B-mode ultrasound (frequency, 12 Mhz; depth, 8 cm; field of view, 14 x 47 mm) (GE  
137 Healthcare Vivid-*i*, Wauwatosa, U.S.A). The same images were utilized to estimate BFlf  
138 fascicle length. The scanning site was determined as the halfway point between the ischial  
139 tuberosity and the popliteal crease, along the line of the BFlf. Once the scanning site was  
140 determined, the distances of the site from various anatomical landmarks were recorded to  
141 ensure its reproducibility for future testing sessions. These landmarks included the ischial  
142 tuberosity, fibula head and the posterior knee joint fold at the mid-point between BF and  
143 semitendinosus tendon. On subsequent visits the scanning site was determined and marked on  
144 the skin and then confirmed by replicated landmark distance measures. All architectural  
145 assessments were performed with participants in a prone position and the hip in a neutral

146 position following at least 5 min of inactivity. Assessments at rest were always performed  
147 first followed by the graded isometric contraction protocol. Assessment of BFlf architecture  
148 at rest was performed with the knee at 0° of knee flexion. Assessment of BFlf architecture  
149 during isometric contractions was always performed with the knee at 0° flexion and preceded  
150 by a maximal voluntary isometric contraction, performed in a custom made device (25). The  
151 graded isometric contractions of the knee flexors were performed in the same device at 25, 50  
152 and 75% of maximum voluntary isometric contraction (MVIC) with the participants shown  
153 the real-time visual feedback of the force produced to ensure that target contraction  
154 intensities were met. Assessment of the MVIC of the knee flexors was undertaken in a prone  
155 position, with both the hip and knee fully extended (0°). Participants were instructed to  
156 contract maximally over a 5-s period, from which the peak force was used to determine the  
157 MVIC.

158 To gather ultrasound images, the linear array ultrasound probe, with a layer of conductive gel  
159 was placed on the skin over the scanning site, aligned longitudinally and perpendicular to the  
160 posterior thigh. Care was taken to ensure minimal pressure was placed on the skin by the  
161 probe as this may influence measurement accuracy (15). Finally, the probe orientation was  
162 manipulated slightly by the sonographer (RGT) if the superficial and intermediate  
163 aponeuroses were not parallel.

164 Analysis was completed off-line (MicroDicom, Version 0.7.8, Bulgaria). For each image, six  
165 points were digitized as described by Blazeovich and colleagues (5). Following the digitizing  
166 process, muscle thickness was defined as the distance between the superficial and  
167 intermediate aponeuroses of BFlf. A fascicle of interest was outlined and marked on the  
168 image. The angle between this fascicle and the intermediate aponeurosis was measured and  
169 given as the pennation angle (Figure 1). The aponeurosis angle for both aponeuroses was



170 determined as the angle between the line marked as the aponeurosis and an intersecting  
171 horizontal line across the captured image (5, 14). Fascicle length was estimated from an  
172 outlined fascicle between the aponeuroses. As the entire fascicle was not visible in the probe  
173 field of view its length was estimated via the following validated equation from Blazeovich  
174 and colleagues (5, 14):

$$175 \quad FL = \sin(AA + 90^\circ) \times MT / \sin(180^\circ - (AA + 180^\circ - PA)).$$

176 Where FL=fascicle length, AA=aponeurosis angle, MT=muscle thickness, AA=aponeurosis  
177 angle and PA=pennation angle.

178 Fascicle length was reported in absolute terms (cm) and also relative to muscle thickness  
179 (fascicle length/muscle thickness). The same assessor (RGT) conducted and analysed all  
180 scans and was blinded to participant identifiers during the analysis. The methodology utilized  
181 in this study to assess the BFlf architectural characteristics has been previously reported by  
182 our laboratory (36).

### 183 **Intervention**

184 The participants performed 6 weeks of either maximal eccentric- or concentric-knee flexion  
185 strength training, with two sessions in the intervention's first week and 3 sessions a week  
186 thereafter on an isokinetic dynamometer (Humac Norm, CSMI, Massachusetts, U.S.A) using  
187 the same range of motion and seat positions configuration as dynamometry testing sessions.  
188 Only one limb received the strength training stimulus, with the contralateral limb acting as a  
189 within-participant control limb. Across the training period the volume (number) of  
190 contractions was increased following the progression below:

- 191 • Week 1:
  - 192 ○ Frequency (days/week) = 2
  - 193 ○ Sets = 4
  - 194 ○ Repetitions = 6

- 195                   ○ Total repetitions = 48
- 196           • Week 2:
- 197                   ○ Frequency (days/week) = 3
- 198                   ○ Sets = 4
- 199                   ○ Repetitions = 6
- 200                   ○ Total repetitions = 72
- 201           • Week 3:
- 202                   ○ Frequency (days/week) = 3
- 203                   ○ Sets = 5
- 204                   ○ Repetitions = 6
- 205                   ○ Total repetitions = 90
- 206           • Week 4:
- 207                   ○ Frequency (days/week) = 3
- 208                   ○ Sets = 5
- 209                   ○ Repetitions = 8
- 210                   ○ Total repetitions = 120
- 211           • Week 5:
- 212                   ○ Frequency (days/week) = 3
- 213                   ○ Sets = 6
- 214                   ○ Repetitions = 6
- 215                   ○ Total repetitions = 108
- 216           • Week 6:
- 217                   ○ Frequency (days/week) = 3
- 218                   ○ Sets = 6
- 219                   ○ Repetitions = 8
- 220                   ○ Total repetitions = 144

221 Each training session was separated by at least 48 hours. Contractions were distributed evenly  
222 across 60°/s and 180°/s. All participants started with two sets of three warm up efforts at  
223 60°/s, in the contraction mode utilized for their training. For all training repetitions, the  
224 concentric training participants were moved to full knee extension (0°) by the investigator  
225 and were instructed to flex their knee as fast as possible through to 90° of knee flexion. The  
226 investigator then returned the lever arm to full knee extension and the subsequent repetition  
227 was completed. This was undertaken until all repetitions were completed in their respective  
228 set, with a 30-s inter-set rest period. The eccentric training participants began with their knee  
229 at 90° of flexion. They were then instructed to maximally flex against the lever arm until full  
230 knee extension was reached (0°). The participant was then instructed to relax, the lever arm  
231 was repositioned to 90° of knee flexion by the investigators and the subsequent contraction

232 was performed. This was undertaken until all repetitions were completed in each set, with a  
233 30-s inter-set rest period. All participants were provided visual and verbal feedback on the  
234 consistency of the torque produced during each repetition. These were compared against  
235 personal best performances, which were known by the participant, to aid motivation. During  
236 the pre-control (*28 days pre-baseline to baseline*), intervention (*baseline to intervention day*  
237 *42*) and detraining periods (*intervention day 42 to post-intervention day 28*), participants  
238 continued their habitual levels of physical activity. The only restriction was to not perform  
239 any other lower limb strength exercises. Finally, training compliance was determined as a  
240 percentage of sessions that were completed within 24 hours of the intended time.

#### 241 **Statistical analysis**

242 All statistical analyses were performed using SPSS version 22.0.0.1 (IBM Corporation,  
243 Chicago, IL). Where appropriate, data were screened for normal distribution using the  
244 Shapiro-Wilk test and homoscedasticity using Levene's test. Greenhouse-Geisser adjustment  
245 was applied when the assumption of sphericity was violated ( $p < 0.05$  for Mauchly's test of  
246 sphericity). At each contraction intensity, a split-plot design ANOVA, with the within-  
247 participant variables being limb (trained or untrained) and time point (*28 days pre-baseline,*  
248 *baseline, intervention day 14, intervention day 21, intervention day 42, post-intervention day*  
249 *28*) and the between-subject variable being group (eccentric or concentric), was used to  
250 compare changes in BFlf architecture throughout the training study. Architectural changes  
251 across the 28 day control period (*28 days pre-baseline to baseline*) were not significant  
252 ( $p > 0.05$ ). Therefore when determining the alterations in BFlf architectural characteristics  
253 following a 6-week intervention, all comparisons were made to *baseline*. Knee flexor peak  
254 torque comparisons, at each contraction velocity, used a similar split-plot design ANOVA,  
255 however, with different time point variables (*baseline, intervention day 42, and post-*  
256 *intervention day 28*). Where significant limb x time x group interactions for architecture and

257 limb x time for knee flexor peak torque were detected, post-hoc t-tests with Bonferroni  
258 adjustments were used to identify which comparisons differed. Significance was set at a  
259  $p < 0.05$  and appropriate Cohen's  $d$  (8) was reported for the comparison effect sizes, with the  
260 levels of effect being deemed small ( $d = 0.20$ ), medium ( $d = 0.50$ ) or large ( $d = 0.80$ ) as  
261 recommended by Cohen (1988).

## 262 **Sample Size**

263 Sample size analysis was completed *a-priori* using G-Power (9). The analysis was based on  
264 the anticipated differences in fascicle length following the strength training intervention. The  
265 effect size was estimated based on the only intervention study to date that has reported  
266 changes in the BFlf architecture (28). That study reported a 33% increase in fascicle length  
267 following the intervention with an approximate effect size of 1.9. Therefore an effect size of  
268 1.2 was deemed as a reasonable starting point. Power was set at 80% with an alpha level of  
269 0.05 returning a calculated sample size of 12 per group. As a cross-reference to confirm the  
270 effect size, fascicle length differences in individuals with a unilateral BFlf strain injury  
271 displayed an effect size of 1.34 when comparing between the previously injured and  
272 contralateral uninjured limb (36).

## 273 **RESULTS**

### 274 **Participants**

275 The two training groups were similar with respect to age, height and body mass (eccentric  
276 training group: age  $21.2\pm 2.7$  y, height  $1.81\pm 0.06$  m, body mass  $77.9\pm 9.3$  kg; concentric  
277 training group: age  $23.4\pm 5.1$  y; height  $1.81\pm 0.07$  m; body mass  $76.2\pm 7.1$  kg). Overall,  
278 compliance rates were acceptable for all participants ( $92\%\pm 2$ ; min=85%; max=100%), with  
279 no differences when comparing the two groups (eccentric training group:  $91\%\pm 2$ ; concentric  
280 training group:  $93\%\pm 1$ ).

### 281 **BFlf architectural comparisons**

#### 282 **Control period, control limb changes and baseline comparisons**

283 A significant limb x time x group interaction effect was found for fascicle length, fascicle  
284 length relative to muscle thickness and pennation angle ( $p<0.001$ ). Post-hoc analyses showed  
285 no BFlf architectural variables changed during the 4-week pre-intervention control period  
286 ( $p>0.05$ ,  $d$  range = 0.03 to 0.17). Similarly, there were no significant differences at any time  
287 point, in the non-training control limbs for any BFlf architectural variables ( $p>0.05$ ,  $d$  range =  
288 0.03 to 0.27). Comparisons of all the BFlf architectural variables at baseline displayed no  
289 significant differences between the concentric and eccentric training group in legs that were  
290 to be trained (i.e. the training leg) ( $p>0.05$ ,  $d$  range = 0.22 to 0.43).

#### 291 **Fascicle length and fascicle length relative to muscle thickness changes**

292 A significant limb x time x group interaction effect was found for fascicle length at all  
293 contraction intensities ( $p<0.001$ ). Post-hoc analysis showed that fascicle length was  
294 significantly longer in the training limb of the eccentric training group ( $p<0.05$ ,  $d$  range: 2.65  
295 to 2.98, Table 1, Figure 2) and significantly shorter in the training limb of the concentric  
296 training group ( $p<0.05$ ,  $d$  range: -1.62 to -0.96, Table 1, Figure 2) after 42 days of the

297 intervention compared to baseline, at all contraction intensities. Additionally there was a  
298 significant limb x time x group interaction effect for fascicle length relative to muscle  
299 thickness ( $p < 0.001$ ). All post-hoc comparisons for the training limbs of each group are  
300 presented in Table 1.

301 Following the 28 day detraining period, fascicle length was significantly reduced in the  
302 training limb of the eccentric training group in comparison to the end of the intervention, at  
303 all contraction intensities ( $p < 0.05$ ,  $d$  range: -1.73 to -1.55, Table 1, Figure 2). Post-hoc  
304 analysis showed that fascicle length in the concentric training group following 28 days of  
305 detraining was no different to that observed end of the intervention, at any contraction  
306 intensity ( $p > 0.05$ ,  $d$  range: 0.15 to 0.67, Table 1, Figure 2). All other post-hoc comparisons of  
307 fascicle length and fascicle length relative to muscle thickness, 28 days following the  
308 intervention period, in the training limbs of both groups are presented in Table 1 and Figures  
309 1 to 4.

### 310 **Muscle thickness and pennation angle changes**

311 No significant limb x time x group interaction effect was found for muscle thickness at any  
312 contraction intensity ( $p > 0.162$ ). However, a significant limb x time x group interaction effect  
313 was detected for pennation angle at all contraction intensities ( $p < 0.001$ ). Post-hoc analysis  
314 showed that pennation angle was significantly reduced in the training limb of the eccentric  
315 training group ( $p < 0.05$ ,  $d$  range: -1.30 to -0.85, Table 1, Figure 2) and significantly increased  
316 in the training limb of the concentric training group ( $p < 0.05$ ,  $d$  range: 1.60 to 2.50, Table 1,  
317 Figure 1 to 4) after 14 days of the intervention compared to baseline, at all contraction  
318 intensities. All other comparisons of pennation angle changes in the training limb of both  
319 groups are presented in Table 1.

320 Pennation angle was not significantly different in the training limb of the eccentric training  
321 group in comparison to the end of the intervention, at any contraction intensity following the  
322 28 day detraining period ( $p>0.05$ ,  $d$  range: -0.55 to 0.02, Table 1, Figure 2). Post-hoc analysis  
323 showed that following the 28 days of detraining, pennation angle of the concentric training  
324 group was no different compared to the end of the intervention, at any contraction intensity  
325 ( $p>0.05$ ,  $d$  range: -0.63 to -0.27, Table 1, Figure 2). All other comparisons of pennation angle  
326 changes following the 28 day detraining period are presented in Table 1.

### 327 **Strength changes**

328 A significant limb x time interaction effect for knee flexor peak torque was found at all  
329 contraction velocities for each group ( $p<0.001$ ). Comparisons at all contraction velocities, at  
330 baseline, displayed no significant differences between the concentric and eccentric training  
331 group ( $p>0.05$ ). Post-hoc analysis also revealed that knee flexor peak torque increased in both  
332 the training limb of the eccentric ( $p<0.05$ ,  $d$  range: 0.63 to 0.78, Table 2) and the concentric  
333 training group ( $p<0.05$ ,  $d$  range: 0.53 to 0.72, Table 2) after 42 days of the intervention, at all  
334 contraction velocities, when compared to baseline. There were no significant differences in  
335 knee flexor peak torque for the untrained limbs of either group after 42 days of the  
336 intervention when compared to baseline, at any contraction velocity ( $p>0.05$ ,  $d$  range = 0.11  
337 to 0.27).

338 There were no significant differences in knee flexor peak torque at any contraction velocity,  
339 in either group when comparing their strength following the 28 day detraining period to the  
340 values after 42 days of the intervention ( $p>0.05$ ,  $d$  range: -0.30 to -0.16, Table 2).  
341 Additionally, knee flexor peak torques at all contraction velocities following the 28-day  
342 detraining period were significantly greater in the training limb of both training groups when  
343 compared to baseline ( $p>0.05$ ,  $d$  range: 0.34 to 0.75, Table 2).

## 344 **DISCUSSION**

345 To the authors' knowledge, this is the first study reporting divergent BFIf architectural  
346 adaptations in response to concentric- or eccentric-strength training. Moreover, it is the first  
347 to provide evidence that eccentric training-induced increases in BFIf fascicle length are  
348 reversed following 28 days of detraining. The main findings were that eccentric strength  
349 training resulted in an increase in estimated BFIf fascicle length and a reduction in pennation  
350 angle, whereas concentric strength training caused reductions in estimated fascicle length and  
351 increases in pennation angle. Additionally, in those who trained eccentrically, a significant  
352 reduction in BFIf fascicle length and a non-significant increase in pennation angle were found  
353 following a 28 day detraining period when compared to the end of the strength training  
354 intervention. In contrast, the concentrically trained group maintained their BFIf architectural  
355 characteristics following 28 days of detraining. Finally, improvements in knee flexor strength  
356 were not specific to training contraction mode, with significant improvements in concentric  
357 and eccentric strength found in both training groups that persisted through the detraining  
358 period.

359 Observations of increases in BFIf fascicle length and a reduction in pennation angle  
360 (measured at rest) following eccentric strength training in the current study (Figure 1) aligns  
361 somewhat with previous literature (28). Potier and colleagues (2009) found a 33% increase in  
362 resting BFIf fascicle length with a non-significant 3.1% reduction in resting pennation angle  
363 following 8 weeks of eccentric strength training. In comparison, the current study saw a  
364 significant 16% increase in resting BFIf fascicle length (the majority of which occurred  
365 within 14 days), with a non-significant 7.5% reduction in resting pennation angle.  
366 Differences in the training modalities employed (leg curl vs isokinetic dynamometry),  
367 intervention length (8 weeks vs 6 weeks) and the site of assessment may explain the different  
368 magnitudes of change reported in these studies. Additionally, no previous literature has



369 examined BFlf architectural alterations during graded isometric contractions, following an  
370 intervention. In the present study, increases in BFlf fascicle length were observed at the end  
371 of the intervention when assessed during all graded isometric contractions in the eccentrically  
372 trained individuals. These increases in fascicle length may occur as a result of the addition of  
373 in-series sarcomeres, as has been shown in rat vastus intermedius muscles after five days of  
374 downhill and presumably eccentric running exercise (18). However, the architectural  
375 alterations seen in this study may not be uniform along the BFlf length. Changes in fascicle  
376 length (4), muscle thickness and anatomical cross sectional area, after strength training  
377 interventions (3), are variable within a muscle. It is possible that the assessment of BFlf  
378 architecture in the current study may have occurred at a point on the muscle where the  
379 changes were less prominent in comparison to other studies (28). Alternatively, changes in  
380 tendon stiffness could theoretically result in altered fascicle lengths, with stiffer tendons  
381 causing an increased tension within the muscle which could then result in the elongation of  
382 resting BFlf fascicle length. Further research is needed to clarify the mechanism responsible  
383 for fascicle length alterations in humans.

384 No previous studies have compared the architectural alterations in the BFlf, following  
385 concentric and eccentric training. However, interventions which have employed concentric-  
386 or eccentric-knee extensor training have reported inconsistent architectural adaptations. Some  
387 have shown a contraction mode specific adaptation similar to that observed in the current  
388 study (10, 29) whilst others have not (3). Additionally knee extensor isometric strength  
389 training at short and long muscle lengths has also been shown to increase fascicle length (22).

390 A range of factors such as the relative maximum load (3, 10), the participant's age and  
391 physical capacity (29) as well as the training stimulus velocity (33) might explain some of the  
392 variance between these results. However it is not known why these alterations in the vastus  
393 lateralis differ to those reported in the current study. It is possible that differences in the

394 structural and functional characteristics of the muscles may account for this variability.  
395 However future research is needed to assist in determining the BFIf adaptive responses to  
396 these and many other variables.

397 The increases in BFIf fascicle length and reductions in pennation angle found in the current  
398 study following an eccentric strength training may have implications for hamstring strain  
399 injury prevention and rehabilitation. Elite athletes with a unilateral history of BFIf strain  
400 injury have shorter fascicles and greater pennation angles on their previously injured limb  
401 when compared to the contralateral uninjured limb (36). Individuals with a history of  
402 hamstring strain injury are at an increased risk of future injury in comparison to those without  
403 a history (24, 26). Therefore if shorter fascicles and greater pennation angles in a previously  
404 injured athlete are partial contributors to the elevated risk of re-injury, then understanding the  
405 most effective methods for altering these architectural characteristics will be of great value.  
406 The current data indicates that the continual application of high-intensity, eccentric-only  
407 strength training should be considered in hamstring rehabilitation and prevention programs in  
408 order to increase BFIf fascicle length and reduce pennation angle. Additionally the current  
409 study results suggest that muscle length in training is possibly not the major factor, as  
410 previously suggested (12), in determining fascicle length changes as long length, concentric  
411 exercise resulted in shortening of fascicle length. Further research is needed to determine how  
412 the combination of both concentric and eccentric contractions during conventional strength  
413 training methods may alter BFIf architecture.

414 The very rapid response of BFIf architectural adaptations supports previous literature which  
415 has found significant increases in fascicle length and pennation angle in the vastus lateralis  
416 within 14 days of the commencement of an eccentrically biased strength training intervention  
417 (31). Furthermore, rat vastus intermedius in-series sarcomere numbers have been shown to  
418 increase within a week of commencing a downhill running protocol (18). In the current study,

419 the majority of fascicle length and pennation angle changes in the eccentric strength training  
420 group occurred within the first 14 days of training, with non-significant changes for the rest  
421 of the intervention (Figure 1 to 4). A similar, but inverse response was found in the  
422 concentric training group after 14 days of training, with non-significant changes for the  
423 remainder of the strength training intervention. These results, along with those from other  
424 studies (3, 31) suggest that early adaptations to strength training are not only from a neural  
425 mechanism (30), but may also be as a result of architectural adaptations.

426 The reported alterations in muscle architecture following periods of detraining are variable,  
427 with most conclusions being drawn from observations of prolonged periods of limb  
428 unloading, some of which show significant reductions in fascicle length, pennation angle and  
429 muscle volume (20, 32), whereas some display no alterations (1). In regards to the detraining  
430 responses following high-intensity eccentric- or concentric-strength training, only one study  
431 has investigated this, 3-months after a 10 week intervention in the vastus lateralis (3).  
432 Blazeovich and colleagues (2007) found no significant alterations in knee extensor strength or  
433 vastus lateralis architectural characteristics following a 3-month detraining period. These  
434 results are inconsistent with the findings from the eccentric training group in the current study  
435 who displayed a significant reduction in BFlf fascicle length and an increase in pennation  
436 angle following 28 days of detraining. In comparison, the concentric group displayed similar  
437 findings to Blazeovich and colleagues (2007), with architectural variables remaining  
438 unchanged following 28 days of detraining (3). The eccentric training group response to the  
439 intervention and then to detraining may be of interest for hamstring strain injury prevention  
440 and rehabilitation interventions as it has been argued that shorter fascicles (i.e. with fewer in-  
441 series sarcomeres) are more prone to muscle damage during high-intensity, eccentric  
442 contractions compared with longer fascicles (11, 19, 36). It remains to be seen what effect  
443 conventional strength training exercises, which possess both concentric and eccentric actions,

444 have on hamstring muscle architecture. In addition, the apparent rapid decrease in fascicle  
445 lengths when the eccentric stimulus is removed would indicate that constant exposure to  
446 eccentric exercise may be important to maintain changes in BFlf architecture following an  
447 intervention period.

448 The strength training interventions in the current study induced significant increases in  
449 concentric and eccentric strength in the training limb of both the concentric and eccentric  
450 training groups (Table 2). Previous research investigating knee flexor strength alterations  
451 following eccentric- or concentric-strength training interventions are variable (13, 28). To the  
452 authors' knowledge, this is the first study to show improvements in both isokinetically  
453 derived concentric and eccentric knee flexor strength independent of training modality.  
454 However, improvements in concentric strength following an eccentric strength training  
455 intervention have been previously reported in the knee flexors, as well as within other muscle  
456 groups (27, 34). There is still some contradictory evidence as to whether a contraction mode-  
457 specific strength adaptation occurs following either concentric- or eccentric-training (3, 10,  
458 29). The current study shows that increases in eccentric strength can be achieved through  
459 long length, concentric strength training in the knee flexors. It is unclear if there might be a  
460 contraction-mode specific adaptation in longer training programs. However the current  
461 findings must be considered in line with the divergent architectural alterations seen between  
462 the two strength training interventions.

463 The authors acknowledge that there are limitations in the current study. Firstly, there are  
464 methodological limitations with the use of two-dimensional ultrasound for the estimation of  
465 BFlf fascicle length. As the field of view utilised in this study does not capture the entire BFlf  
466 fascicle, estimation is required. The equation utilised in this study has been validated against  
467 cadaveric samples (14), however it must be recognized that there is still a level of error  
468 associated with estimations of BFlf fascicle length. Future studies should consider extended

469 field of view ultrasound methods (23) to reduce the level of error when estimating muscle  
470 fascicle length. Secondly, the assessment of muscle architecture was only performed on the  
471 BFlf and did not include the other knee flexors. Therefore it is unknown what adaptations  
472 these other muscles displayed following the intervention and detraining period. However, as  
473 the BFlf is the most commonly strain injured hamstring muscle (16), the alterations following  
474 concentric and eccentric strength training interventions were of interest from a hamstring  
475 strain injury risk and rehabilitation perspective. Finally, the training stimulus was provided  
476 with an even distribution of the number of contractions across both slow and fast isokinetic  
477 velocities. As vastus lateralis architectural adaptations have been shown to be velocity  
478 dependent (33), it is not possible to determine if the changes in this cohort and muscle are due  
479 to the velocities utilised. The aim of this study was to investigate the effect of contraction  
480 mode, not velocity, on BFlf architectural changes as this may have greater implications for  
481 hamstring strain injury prevention and rehabilitation. Further research is needed to determine  
482 if there is a contraction velocity-specific adaptation in the knee flexors following a  
483 concentric- or eccentric-strength training intervention.

484 In conclusion, the current study reports rapid, contraction-mode specific alterations in BFlf  
485 architecture following 6 weeks of either eccentric or concentric strength training  
486 interventions. Further, 28 days of detraining resulted in BFlf architectural characteristics  
487 returning to baseline levels in individuals who had completed eccentric training, whilst  
488 detraining had no influence on the BFlf architectural characteristics in those who completed  
489 concentric strength training. The findings of the current study provide insight into BFlf  
490 architectural alterations following concentric and eccentric strength training interventions.  
491 These results may have implications for hamstring injury prevention and rehabilitation  
492 programs which might consider architectural alterations to training interventions as a factor  
493 that might mitigate risk of future injury.

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495 N/A

496 **CONFLICT OF INTEREST**

497 The authors report that this study was not funded at that no conflict of interest exists. Results  
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501 **REFERENCES**

- 502 1. Abe T, Kawakami Y, Suzuki Y, Gunji A, Fukunaga T. Effects of 20 days bed rest on  
503 muscle morphology. *J Gravit Physiol.* 1997;4(1):S10-4.
- 504 2. Blazevich AJ. Effects of physical training and detraining, immobilisation, growth and  
505 aging on human fascicle geometry. *Sports Med.* 2006;36(12):1003-17.
- 506 3. Blazevich AJ, Cannavan D, Coleman DR, Horne S. Influence of concentric and  
507 eccentric resistance training on architectural adaptation in human quadriceps muscles. *J Appl*  
508 *Physiol (1985).* 2007;103(5):1565-75.
- 509 4. Blazevich AJ, Gill ND, Bronks R, Newton RU. Training-specific muscle architecture  
510 adaptation after 5-wk training in athletes. *Med Sci Sports Exerc.* 2003;35(12):2013-22. Epub  
511 2003/12/04. doi: 10.1249/01.MSS.0000099092.83611.20.
- 512 5. Blazevich AJ, Gill ND, Zhou S. Intra- and intermuscular variation in human  
513 quadriceps femoris architecture assessed in vivo. *J Anat.* 2006;209(3):289-310.
- 514 6. Bodine SC, Roy RR, Meadows DA, et al. Architectural, histochemical, and  
515 contractile characteristics of a unique biarticular muscle: the cat semitendinosus. *J*  
516 *Neurophysiol.* 1982;48(1):192-201.

- 517 7. Brockett CL, Morgan DL, Proske U. Predicting hamstring strain injury in elite  
518 athletes. *Med Sci Sports Exerc.* 2004;36(3):379-87.
- 519 8. Cohen D. *Statistical power analysis for the behavioral sciences.* Hillsdale (NJ):  
520 Erlbaum; 1988. p 75.
- 521 9. Faul F, Erdfelder E, Lang AG, Buchner A. G\*Power 3: a flexible statistical power  
522 analysis program for the social, behavioral, and biomedical sciences. *Behav Res Methods.*  
523 2007;39(2):175-91.
- 524 10. Franchi MV, Atherton PJ, Reeves ND, et al. Architectural, functional and molecular  
525 responses to concentric and eccentric loading in human skeletal muscle. *Acta Physiol (Oxf).*  
526 2014;210(3):642-54.
- 527 11. Fyfe JJ, Opar DA, Williams MD, Shield AJ. The role of neuromuscular inhibition in  
528 hamstring strain injury recurrence. *J Electromyogr Kinesiol.* 2013;23(3):523-30.
- 529 12. Guex K, Millet GP. Conceptual framework for strengthening exercises to prevent  
530 hamstring strains. *Sports Med.* 2013;43(12):1207-15.
- 531 13. Kaminski TW, Wabbersen CV, Murphy RM. Concentric versus enhanced eccentric  
532 hamstring strength training: clinical implications. *J Athl Train.* 1998;33(3):216-21.
- 533 14. Kellis E, Galanis N, Natsis K, Kapetanios G. Validity of architectural properties of the  
534 hamstring muscles: correlation of ultrasound findings with cadaveric dissection. *J Biomech.*  
535 2009;42(15):2549-54.
- 536 15. Klimstra M, Dowling J, Durkin JL, MacDonald M. The effect of ultrasound probe  
537 orientation on muscle architecture measurement. *J Electromyogr Kinesiol.* 2007;17(4):504-  
538 14.
- 539 16. Koulouris G, Connell DA, Brukner P, Schneider-Kolsky M. Magnetic resonance  
540 imaging parameters for assessing risk of recurrent hamstring injuries in elite athletes. *Am J*  
541 *Sports Med.* 2007;35(9):1500-6.

- 542 17. Lieber RL, Ward SR. Skeletal muscle design to meet functional demands. *Philos*  
543 *Trans R Soc Lond B Biol Sci.* 2011;366(1570):1466-76.
- 544 18. Lynn R, Morgan DL. Decline running produces more sarcomeres in rat vastus  
545 intermedius muscle fibers than does incline running. *J Appl Physiol (1985).* 1994;77(3):1439-  
546 44.
- 547 19. Morgan DL. New insights into the behavior of muscle during active lengthening.  
548 *Biophys J.* 1990;57(2):209-21.
- 549 20. Narici M, Cerretelli P. Changes in human muscle architecture in disuse-atrophy  
550 evaluated by ultrasound imaging. *J Gravit Physiol.* 1998;5(1):P73-4.
- 551 21. Narici MV, Flueck M, Koesters A, et al. Skeletal muscle remodeling in response to  
552 alpine skiing training in older individuals. *Scand J Med Sci Sports.* 2011;21 Suppl 1:23-8.
- 553 22. Noorkoiv M, Nosaka K, Blazevich AJ. Neuromuscular adaptations associated with  
554 knee joint angle-specific force change. *Med Sci Sports Exerc.* 2014;46(8):1525-37.
- 555 23. Noorkoiv M, Stavnsbo A, Aagaard P, Blazevich AJ. In vivo assessment of muscle  
556 fascicle length by extended field-of-view ultrasonography. *J Appl Physiol (1985).*  
557 2010;109(6):1974-9.
- 558 24. Opar D, Williams M, Timmins R, Hickey J, Duhig S, Shield A. Eccentric hamstring  
559 strength and hamstring injury risk in Australian Footballers. *Med Sci Sports Exerc.*  
560 2015;47(4):857-65.
- 561 25. Opar DA, Piatkowski T, Williams MD, Shield AJ. A novel device using the nordic  
562 hamstring exercise to assess eccentric knee flexor strength: a reliability and retrospective  
563 injury study. *J Orthop Sports Phys Ther.* 2013;43(9):636-40.
- 564 26. Orchard JW, Seward H, Orchard JJ. Results of 2 decades of injury surveillance and  
565 public release of data in the Australian Football League. *Am J Sports Med.* 2013;41(4):734-  
566 41.



- 567 27. Paddon-Jones D, Leveritt M, Lonergan A, Abernethy P. Adaptation to chronic  
568 eccentric exercise in humans: the influence of contraction velocity. *Eur J Appl Physiol.*  
569 2001;85(5):466-71.
- 570 28. Potier TG, Alexander CM, Seynnes OR. Effects of eccentric strength training on  
571 biceps femoris muscle architecture and knee joint range of movement. *Eur J Appl Physiol.*  
572 2009;105(6):939-44.
- 573 29. Reeves ND, Maganaris CN, Longo S, Narici MV. Differential adaptations to eccentric  
574 versus conventional resistance training in older humans. *Exp Physiol.* 2009;94(7):825-33.
- 575 30. Selvanayagam VS, Riek S, Carroll TJ. Early neural responses to strength training. *J*  
576 *Appl Physiol (1985).* 2011;111(2):367-75.
- 577 31. Seynnes OR, de Boer M, Narici MV. Early skeletal muscle hypertrophy and  
578 architectural changes in response to high-intensity resistance training. *J Appl Physiol (1985).*  
579 2007;102(1):368-73.
- 580 32. Seynnes OR, Maganaris CN, de Boer MD, di Prampero PE, Narici MV. Early  
581 structural adaptations to unloading in the human calf muscles. *Acta Physiol (Oxf).*  
582 2008;193(3):265-74.
- 583 33. Sharifnezhad A, Marzilger R, Arampatzis A. Effects of load magnitude, muscle  
584 length and velocity during eccentric chronic loading on the longitudinal growth of the vastus  
585 lateralis muscle. *J Exp Biol.* 2014;217(Pt 15):2726-33.
- 586 34. Shepstone TN, Tang JE, Dallaire S, Schuenke MD, Staron RS, Phillips SM. Short-  
587 term high- vs. low-velocity isokinetic lengthening training results in greater hypertrophy of  
588 the elbow flexors in young men. *J Appl Physiol (1985).* 2005;98(5):1768-76.
- 589 35. Thelen DG, Chumanov ES, Hoerth DM, et al. Hamstring muscle kinematics during  
590 treadmill sprinting. *Med Sci Sports Exerc.* 2005;37(1):108-14.

- 591 36. Timmins R, Shield A, Williams M, Lorenzen C, Opar D. Biceps femoris long head  
592 architecture: a reliability and retrospective injury study. *Med Sci Sports Exerc.*  
593 2015;47(5):905-13.
- 594 37. Timmins RG, Opar DA, Williams MD, Schache AG, Dear NM, Shield AJ. Reduced  
595 biceps femoris myoelectrical activity influences eccentric knee flexor weakness after repeat  
596 sprint running. *Scand J Med Sci Sports.* 2014;24(4):e299-e305.
- 597 38. Yu B, Queen RM, Abbey AN, Liu Y, Moorman CT, Garrett WE. Hamstring muscle  
598 kinematics and activation during overground sprinting. *J Biomech.* 2008;41(15):3121-6.
- 599

600 Figure 1: A two dimensional ultrasound image of the biceps femoris long head. This image of  
601 the biceps femoris long head was taken along the longitudinal axis of the posterior thigh.  
602 From these images it is possible to determine the superficial and intermediate aponeuroses,  
603 muscle thickness, angle of the fascicle in relation to the aponeurosis. Estimates of fascicle  
604 length can then be made via trigonometry using muscle thickness and pennation angle.

605 Figure 2: Changes in the architectural characteristics of the BFlf when assessed at rest in the  
606 trained limb and the contralateral untrained limb of both groups following 14, 21 and 42 days  
607 of the training intervention and following the detraining period (*day 70*). A) fascicle length  
608 B) pennation angle C) muscle thickness D) fascicle length relative to muscle thickness. Error  
609 bars illustrate the standard deviation. \*=p<0.05 vs Day 0, \*\* = p<0.001 vs Day 0, ## =  
610 p<0.001 vs Day 42.

611

612 Table 1: Changes in the BFlf architectural characteristics in the training limb of each group at  
613 the start (day 0), after 14, 21 and 42 days of the training intervention as well as following the  
614 detraining period (day 70). All data represented as mean±SD unless otherwise stated. SD =  
615 standard deviation, MT = muscle thickness, cm = centimetres, PA = pennation angle, RFL =  
616 fascicle length relative to muscle thickness, FL = fascicle length, MVIC = maximum  
617 voluntary isometric contraction. \*=p<0.05 vs Day 0, \*\* = p<0.001 vs Day 0, # = p<0.05 vs  
618 Day 42, ## = p<0.001 vs Day 42.

619 Table 2: Changes in concentric and eccentric knee flexor peak torque at various contraction  
620 velocities in the training limb of each group before (day 0) and after the training intervention  
621 (day 42) as well as following the detraining period (day 70). All data represented as  
622 mean±SD unless otherwise stated. SD = standard deviation, °/s = degrees per second.  
623 \*=p<0.05 vs Day 0, \*\* = p<0.001 vs Day 0.

