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- 34 Abstract:
- 35

36 *Objectives:* Investigate the determinants of hamstring fascicle length within professional rugby
 37 league players.

38 *Design:* Retrospective cohort study

39 Method: Thirty-three athletes underwent a testing during the early and late pre-season periods.
40 Fascicle length measurements of biceps femoris, 3D kinematics and elapsed time-periods at
41 thigh angular velocities between 20deg/s to peak velocity during a single-leg eccentric
42 hamstring strength test, GPS-derived running loads, age and previous injury history were all
43 recorded. Fixed effect determinants for fascicle length were analyzed using multiple linear
44 regression.

45 Results: Significant determinants of hamstring fascicle length were observed. Multivariate 46 regression analysis showed modifiable factors including chronic running volumes >80% of 47 measured peak speed collectively explained 43% of the variability in the fascicle length data, 48 whilst peak eccentric strength-related and elapsed time under load from 20deg/s to peak thigh 49 angular velocity collectively contributed an additional 44%. Chronic running volumes >90% 50 of individually measured peak speed and the 'break angle' during a Nordic eccentric 51 contraction were not significant contributors to the final model. Non-modifiable risk factors 52 (age and previous injury) contributed the remaining 13%.

53 *Conclusions:* Managing high speed running exposure as well as eccentric strength training 54 allows for ~90% of the controllable determinants in fascicle length within elite athlete 55 populations. An important contributor to the explained variability within fascicle length 56 (superseded only by chronic speed exposure and peak eccentric strength) was an athletes ability 57 to achieve a prolonged contraction at long lengths during eccentric strength training rather than 58 the angle of failure during the contraction in itself.

#### 59 Keywords: Hamstring, Fascicle, Injury, Speed, Strength, Prevention, Sport

## 60 **Practical Implications**

61 •	Using factors that are readily available in elite sporting settings, it was possible to
62	determine ~90% of the variability in biceps femoris long head fascicle length with a
63	multiple linear regression. These factors included chronic running exposure >80% of a
64	relative maximum velocity, peak eccentric strength (during the Nordic) and time under
65	load at longer leg lengths in the Nordic. Non-modifiable factors (age and previous
66	history) also contributed to the explained variability in fascicle length.

- 67 Chronic running exposure >90% of relative maximal velocity and the 'break angle'
  68 during a Nordic effort were not statistically significant contributors to determining
  69 fascicle length.
- These findings give practitioners the option to monitor alternative variables (instead of
   fascicle length itself) and be able to approximate (around 90%) of the impact it may
   have on fascicle adaptations in elite athletes.

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### 75 Introduction

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Hamstring strain injuries (HSI) are the most common non-contact lower limb injuries
in team sports that involve sprinting, kicking, jumping or high-speed movements<sup>10</sup>. Increases
in overall injury rates negatively influence team<sup>8</sup> and individual performances<sup>28</sup>, which have
negative financial consequences for sporting organizations and athletes<sup>10</sup>. As such, identifying
factors associated with HSI have important applications to practitioners in team sport.

82 A number of non-modifiable risk factors for HSI have been identified previously, most prominently, increasing age and previous injury<sup>2,9</sup>. However, in recent times, a greater 83 84 emphasis has been placed on modifiable risk factors and appropriate interventions, which may lead to reductions in an athlete's risk of HSI <sup>25</sup>. Of these modifiable risk factors, eccentric 85 hamstring strength has received significant attention <sup>1,3,19,20</sup>, with low levels of eccentric 86 87 hamstring strength reported to increase the risk of future hamstring injury in athletes from different football codes<sup>4,13</sup>. Recently, it has been reported that elite footballers with biceps 88 89 femoris long head (BFlh) muscle fascicles shorter than 10.56cm (determined using a receiver 90 operating characteristic curve) were approximately four times more likely to suffer a hamstring injury in the subsequent season compared to athletes with longer fascicles<sup>24</sup>.. These data 91 92 suggest that interventions aimed at increasing BFlh fascicle lengths and eccentric knee flexor strength should be prioritized in hamstring injury prevention programs<sup>14</sup>. Furthermore, it has 93 94 been reported that the 'break-point' angle (i.e. the point that a steady state lowering during a Nordic eccentric exercise cannot be sufficiently controlled) achieved during Nordic hamstring 95 lowers was: 1) positively correlated to eccentric hamstring strength<sup>19</sup> and 2) able to be used as 96 a field-based assessment of eccentric hamstring strength<sup>12,19</sup>. However, the applicability of this 97 98 measure to elite sport is still unknown.

99 The risk of future HSI has also been related with spikes in high-speed (>24km/hr.) running volumes, which are relative to each athlete's regular performance<sup>7,18</sup>. However, both 100 101 over- and under-exposure to maximum speed (>85% of maximum velocity) efforts and volume 102 (i.e. distance covered) is associated with the greatest risk of non-contact lower limb injury in 103 professional Australian footballers<sup>15,21</sup>. Although there is an association between running 104 exposure and the risk of HSI, the independent use of running variables to predict future HSI 105 may have limited clinical value, where multiple factors (including eccentric strength and fascicle length) may be needed to determine the probability of a future HSI <sup>16</sup>. 106

As such, the purpose of this study was to evaluate the influence of elite physical training
variables on fascicle length changes in professional rugby league players. These variables
included peak hamstring eccentric strength and quality of such a movement (i.e. 'break angle'),
as well as running exposure, age, and injury history across a single-season in professional rugby
league players.

#### 112 Methods

113 The study received ethical approval from the Human Research Ethics Committee 114 (approval number 2018-135H). Thirty-three elite rugby league players (mean age: 23.9±3.9 115 years, mean body mass: 98.6±9.6kg, mean height: 187±4.6cm) underwent a comprehensive 116 performance battery on three separate occasions, separated by a minimum of 56 days (i.e. 8 117 weeks); December 2017 (early pre-season), February 2018 (late pre-season) and May 2018 (in-118 season). The following was tested on each occasion: 1) peak force output during a single-leg 119 Nordic hamstring exercise using a Nordbord (Vald Performance, Albion QLD, Australia); 2) 120 motion analysis during a single-leg Nordic hamstring exercise using an 8-camera 3D motion 121 capture system (Vicon, Oxford UK); and 3) measurement of BFlh fascicle length. In addition, 122 Global Positioning System (GPS)-derived distance covered >80% and 90% of each athlete's 123 individual peak speed over the preceding 28 (28-day chronic load) and 56 (56-day chronic load) days prior to each test was recorded via wearable GPS technology, which has
demonstrated accuracy and reliability for measuring instantaneous velocity (Catapult Sports,
Melbourne Victoria, Australia)<sup>27</sup>. Anthropometric data and previous injury history were also
recorded by qualified physiotherapists.

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129 An experienced exercise physiologist performed all motion analysis and hamstring 130 strength testing, whilst fascicle length testing was undertaken by a reliable assessor on each occasion. The assessor who measured fascicle length has previously reported reliability metrics 131 132 with intraclass correlations ranging between 0.96 to 0.97 and typical error as a percentage of 133 coefficient of variation less than 3.4% (range 2.1 to 3.4%)<sup>26</sup>. Injury history and anthropometric 134 data were collated by qualified physiotherapists. For the purposes of this investigation, the 135 dominant leg was considered the participant's preferred leg when kicking a ball. Eccentric 136 hamstring strength testing and motion analysis (for the break-point analysis) were captured 137 simultaneously, with fascicle length measured before any exercise on the same day. Chronic 138 running loads greater than 80, and 90% of each player's maximum velocity were collated from 139 the preceding 28, and 56 days prior to each respective test.

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141 The hamstring strength testing device (Vald Performance, Albion, Queensland, 142 Australia) and 3D motion capture (Vicon, Oxford UK) were set-up as per the manufacturer's 143 recommendations. Lower body plug-in gait was used for motion capture. Prior to testing, each 144 participant was allowed a five-minute warm up consisting of one set of five double-leg 145 repetitions as a warm-up. Testing consisted of one set of three single-leg maximum eccentric 146 contractions on each side, with the dominant leg tested first (e.g. participants complete 3 efforts 147 of a single-leg Nordic on their dominant leg and then undertook the same testing on their non-148 dominant leg – supplementary video 1). All athletes had undertaken single-leg Nordics for at 149 least 3 months prior to the testing and were familiar with the exercise and how it differs from 150 the double-leg version. During all efforts, the participants were advised to maintain a 151 neutral/extended hip position. Average peak force (Newtons) across the three repetitions was 152 recorded for each testing period. In addition, the corresponding knee angle of the tested limb 153 at the time of reaching the below thigh angular velocities, was recorded for each maximal 154 effort: 20deg/sec (corresponding to the start of the forward movement), 60deg/sec 155 (corresponding to the period when the athlete began to 'accelerate' during the eccentric 156 movement, and *peak angular velocity* which represented loss of control of the movement. 157 Additionally, the elapsed time period (milliseconds) between 20-60deg/sec and 20-peak 158 velocity were recorded to account for the time under load during the contraction. The results of 159 the testing parameters are summarised in Table 1.

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161 The processes used for the collection of BFlh architecture has been previously described<sup>26</sup>. The extrapolation technique, whilst not a direct measure of fascicle length, has 162 163 been successfully validated against cadaveric tissues and as such is considered a robust way of estimating fascicle lengths<sup>11</sup>. Muscle thickness, pennation angle and fascicle length of the BFlh 164 165 were determined utilising two-dimensional, B-mode ultrasound (frequency 12MHz; depth 166 8cm; field of view, 14 x 47mm) (GE Healthcare Vivid-I, Wauwatosa, WI). The site of 167 assessment was determined as halfway between the ischial tuberosity and the popliteal crease, 168 along the line of the BFlh. All assessments were undertaken in a prone position with both the 169 hip and knee extended, with the participant having undertaken 5mins of inactivity. The 170 ultrasound probe, with a layer of conductive gel, was placed perpendicular to the posterior 171 thigh on top of the measured scanning site. The orientation of the probe was then manipulated by a skilled assessor, with published reliability, until a clear image was obtained<sup>26</sup>. 172

173	Once the images were collected, analysis was undertaken off-line (MicroDicom,
174	Version 0.7.8, Bulgaria). For each image, fascicle length estimation was undertaken using the
175	equation which was validated against cadaveric tissues <sup>11</sup> . The equation used was:
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177	$FL = sin(AA + 90^{\circ}) x MT/sin [180^{\circ} - (AA + 180^{\circ} - PA)]$
178	where:
179	FL = fascicle length, $AA$ = aponeurosis angle, $MT$ = muscle thickness and $PA$ =
180	pennation angle.
181	Fascicle length was reported in absolute terms (cm) from a single image and fascicle. The
182	results of these tests are presented in Table 1.
183	These data were collected from training within the previous 28 and 56 day periods prior to each
184	respective testing block. The peak speed (m.s <sup>-1</sup> ) achieved between tests and average 7-day
185	running volume (m) greater than 80%, and 90% of peak speed was calculated for the preceding
186	28, and 56 days. The results of these data are summarised in Table 1. This study utilized a
187	convenient sample of 33 players and was undertaken in an exploratory manner. Statistical
188	analysis was performed using R-Studio Statistical package (version 1.1.423).
189	
190 191	<b>Results</b> Thirty-three athletes were included in the final analysis. The group included outside backs
192	(n=16), edge (n=6) and middle players (n=11). Results across the group indicated fascicle
193	lengths of 10.11cm at testing 1 (pre-season), 10.65cm at testing 2 (late-pre-season), and
194	10.52cm at testing 3 (in-season; Table 1). Nordic force and motion analysis results indicated a

- 195 mean Nordic peak force output of 407.3N / 4.16N/kg (IQR = 321-471; 3.52-4.72), 623ms (IQR
- 196 = 555-723) from start of forward movement until peak thigh angular velocity during the

197 eccentric contraction, and 37.7deg (IQR = 42-32) knee angle at the time of peak angular198 velocity.

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Running loads during the study period are indicated in Table 1. Results here indicate a mean maximum velocity of  $8.74 \text{m/s}^{-1}$  (IQR = 8.3-9.2) with mean chronic load >80% of the measured maximum speed 76.8m (IQR = 33.3-107.8) and 58.9m (IQR = 31.1-79.5) for the preceding 28 and 56-day periods, respectively. Mean speed volumes >90% of the measured maximum speed measured 14 m (IQR = 3.3-20.0) and 9.7m (IQR = 3.4-13.7) for the preceding 28 and 56-day periods, respectively.

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207 To examine the fixed-effect determinants of fascicle length, a multiple linear regression 208 analysis was performed. This involved a backward stepwise regression from the full model (all 209 variables included) to arrive at the final model. The analysis of variance is presented in 210 Supplementary Table 2. This indicates that the predictors used in the final analysis to be 211 statistically useful contributors to the final model.. This indicates that the predictors used in the 212 final analysis to be statistically useful contributors to the final model. The summary of 213 coefficients for the final model is indicated in Supplementary Table 1. The adjusted R-squared 214 value for the final model on the current data set was 50.6 (F-value 8.62 on 9 and 58 df, p-value 215 = 4.56e-08), indicating that 50.6% of the explained variability in fascicle length within the 216 dataset was due to the variables included in the final model. The relative contribution of each 217 variable to the final model is indicated in Figure 1 [INSERT FIGURE 1 NEAR HERE]. The 218 most important contributor to fascicle length within the observed dataset was running volume 219 (measured in meters) >80% of the athletes measured maximum velocity (30%). Peak Nordic 220 force output (27%) and elapsed time under load at long lengths (17%) rounded out the three 221 highest contributors to fascicle length changes. Peak speed (13%), previous injury (8%) and age (5%) were other statistically significant contributors to the observed variability in fascicle
length within this dataset. Running volumes >90% and angle-specific thigh angular velocities
(20deg/s, 60deg/s and angle of peak thigh angular velocity) were not statistically significant
determinants of fascicle length within this data set.

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The model assumptions (residuals plots) are highlighted in Figure 2. The model assumptions are that the residuals are independent and are normally distributed, centred around zero and have a constant variance ( $\varepsilon \sim N(0,\sigma^2)$ ). The observations in the Residuals vs Fitted plot, Scale-Location Plot and Residuals vs Leverage Plots (Figure 2) [INSERT FIGURE 2 NEAR HERE] are centred around zero with relatively constant variance. In the normal QQ plot (Figure 3) there is some slight variance from the straight line particularly at the tails, and two observations are outside 2 standardised residuals suggesting they are potential outliers.

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### 235 Discussion

237 This is the first study in professional team sport athletes to identify determinants of 238 BFlh fascicle length. We demonstrated relative chronic running loads >80% of maximum 239 velocity explained around 43% of the variability in fascicle length, whilst the often-240 recommended threshold >90% was not a statistically significant contributor. Our findings also 241 demonstrated that peak eccentric hamstring force was associated with 27% of the variance in 242 BFlh fascicle length. When combined with prolonged eccentric time under tension at long 243 muscle lengths (17%) these two factors described around 44% of the explained variability in 244 fascicle length. Collectively, these findings may help guide conditioning and prevention 245 strategies for athletes in the future. If practitioners are unable to monitor fascicle length 246 changes, managing chronic running loads >80% of maximum velocity as well as eccentric strength training may help estimate around 90% of the controllable determinants in BFlh 247 248 fascicle length in their athletes.

249 Peak speed (13% of the observed variability) and running volume > 80% of maximum 250 velocity during the preceding 56-day period (30% of the observed variability) were the largest 251 collective contributors to the explained variability in fascicle length. Previous literature has 252 advocated maintenance of chronic high speed running loads in the prevention of hamstring strain injury<sup>5,17</sup>. Although regular exposure >90% of the measured maximum velocity is often 253 recommended within high performance environments for HSI prevention<sup>22</sup>, the results of this 254 255 study suggest that running loads at this velocity may not may not be statistically associated with longer fascicle lengths. In practical terms, each 2.5ms<sup>-1</sup> increase in peak velocity within 256 257 this cohort was associated with 0.94cm longer fascicle length. Although the findings of this 258 study suggests that regular exposure >80% of an athletes maximum velocity might be 259 associated with longer fascicle lengths in professional athletes, the volume required for a 260 meaningful increase in BFlh from was practically very high, indicating a larger dataset is likely 261 needed to confirm this finding.

262 Peak eccentric strength was the second most important contributor to the explained 263 variability of fascicle length (27%). Previous research has affirmed the benefits of eccentric training in optimising fascicle length adaptation<sup>1,3,14,20</sup>. Within this cohort, an increase in peak 264 265 force of 150N was associated with an additional 1.1cm longer fascicle. The current study found 266 that time under load at longer lengths (between 60deg/sec and peak thigh angular velocity) 267 during a single-leg eccentric hamstring exercise (17% of the explained variability in fascicle 268 length), not the 'break point' angle of the exercise (i.e. angle of loss of control) to be statistically associated with longer fascicle lengths. Previous literature<sup>12,19,22,23</sup> has explored the concept of 269 270 the break angle as a measure of potentially assessing HSI risk. Whilst the break point angle 271 wasn't associated with BFlh fascicle lengths, it would appear that it is the combined ability to 272 sustain an elapsed time under supramaximal load that has the strongest correlation with fascicle 273 length. In practical terms, increasing time under load by 100ms between 20deg/sec and 60deg/sec was associated with a 2.35cm longer BFlh fascicle length. This may represent a useful addition to strength training programming in HSI prevention. Interestingly, longer fascicles within this cohort was associated with a lower ratio force output per kg bodyweight with during the Nordic (1 N/kg reduction associated with an increase of 0.75cm BFlh fascicle length). Confirmation within a larger dataset is needed, though in practical terms this might indicate that maximal force output might be more favourably associated with longer fascicle lengths than force per unit of bodyweight.

281 Age (5%) and previous injury (8%) were the final contributors to the explained 282 variability in fascicle length within the dataset. Having a previous HSI and increasing age have 283 been extensively reported to augment the likelihood of an injury occurring <sup>2,9</sup>. Although the 284 results of this study reaffirm the importance of these factors, it is encouraging that the majority 285 of the model relating to longer fascicle lengths is explained by factors which can be modified 286 through various interventions, allowing practitioners the ability to potentially address an 287 athletes risk. Previous history was associated with a 0.3cm shorter fascicle length, and an 288 athlete who was 10 years older was associated with 0.23cm shorter fascicles, both largely 289 within the measurement error of BFlh fascicle length..

290 There are limitations associated with this study. Firstly, the data was only collected over 291 a single professional season. Although statistically significant influences on fascicle length 292 changes were observed, we were able to explain just over 50% of the total variability in fascicle 293 length within this dataset, meaning that there are other statistical influences on fascicle length 294 changes which we did not account for in this study. Although we conducted an analysis in order 295 to achieve sufficient power within the study, continued observation over multiple seasons will 296 further strengthen the predictive capability of these models, and further research should seek 297 to explore additional influences on fascicle length such as heavy isometrics and other hamstring 298 strength exercises as well as targeted flexibility and mobility work which has also been 299 advocated in HSI injury prevention. Secondly, the measure of fascicle length is an estimation 300 made from a validated equation. This is due to the small transducer field of view being unable 301 to capture an entire BFlh fascicle. However, whilst the results are still an estimation, the 302 methodology and equation employed has been validated against cadaveric samples and shows excellent agreement between dissection and estimation methods<sup>11</sup>. Ideally transducers with 303 304 larger fields of view or panoramic functions would be used, however such equipment and 305 techniques are not available in our laboratory.

#### 306 Conclusions

307 Significant determinants of hamstring fascicle length were observed over a single professional 308 rugby league season. Chronic running load >80% of maximum speed (28 days and 56 days 309 combined) and overall maximum speed explained 43% of the observed variability in fascicle 310 length, whilst strength-related variables collectively contributed an additional 44%. Non-311 modifiable risk factors (age and previous injury) collectively contributed the remaining 13%. 312 Future research should examine absolute predictive thresholds for physical performance-based 313 tests and re-injury risk reduction, as well as seek to include additional training modalities over 314 and above the ones included in this study as means of further optimizing the explained 315 influences on hamstring fascicle length for hamstring injury prevention in professional athletes.

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#### 317 **Practical Implications**

- Using multiple linear regression analysis, statistically significant determinants of
   fascicle length were observed in elite rugby league athletes over a single professional
   season.
- Based on the results of this study, modifiable risk factors collectively represented close
   to 90% of the explained variability in fascicle length. These factors included chronic

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323	speed exposure >80% of measured maximum running velocity, peak eccentric strength
324	and time under load at longer leg lengths. Non-modifiable factors (age and previous
325	history) collectively accounted for the remaining explained variability. Speed
326	thresholds > 90% of individual maximum velocity and the 'break angle' during a
327	Nordic eccentric contraction were not statistically significant contributors.
328 •	Inclusion of these training strategies may help optimize hamstring injury prevention
329	training in the future
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- Figure 1: Average biceps femoris fascicle length results across the three testing time points
- 435 Figure 2: Contributors to biceps femoris fascicle length from the linear regression analysis
- 436437 Figure 3: Residuals plots for the final model

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# **Relative Importance Metrics**





Table 1: Fascicle length, eccentric hamstring strength, Nordic performance measures as well as and GPS speed and distance measures in elite Rugby League athletes.

	Fascicle	Eccentric		Elapsed Time During		Knee Angle At Specific Thigh			GPS Measures				
	Length	Hamstring		The Nordic		Angular Velocity (Deg)							
		Measures		(Milliseconds)									
	Average	Peak	N/kg	20-60deg	20-Peak	20deg/s	60deg/s	Peak	Max	>80%	>80%	>90%	>90%
	( <b>cm</b> )	Force	BW		Velocity			Velocity	Speed	(28	(56	(28	(56 day)
		(N)						(deg/s)	( <b>m/s</b> <sup>-1</sup> )	day)	day)	day)	
Min	8.99cm	203.7	2.34	118.3	156.7	93.35	82.28	64.20	6.981	0.00	3.439	0.000	0.00
1 <sup>st</sup> Qtr.	9.91cm	321.5	3.52	288.3	554.6	84.93	71.66	41.88	8.338	33.29	31.055	3.263	3.414
Median	10.44cm	387.1	3.93	365.0	636.7	78.96	65.75	36.71	8.777	60.54	45.720	10.453	6.434
Mean	10.34cm	407.3	4.16	369.1	623.3	80.43	67.26	37.70	8.743	76.82	58.918	13.957	9.701
3 <sup>rd</sup> Qtr.	10.74cm	471.2	4.72	430.0	723.3	76.17	61.30	32.00	9.248	107.82	79.463	19.974	13.685
Max	11.48cm	743.7	7.36	681.7	936.7	25.53	20.37	12.67	10.195	327.00	231.866	58.565	41.006
										Measured in metres			S

cm = centimetres, n = newtons of force, N/kg BW = newtons of force relative to body weight, deg/s = degrees per second, deg = degrees, GPS = Global Positioning System, m/s-<sup>1</sup> = metres per second squared

Supplementary Table 1: Coefficients of multiple linear regression:

	<b>Estimate</b>	Std.Error	<u>t-value</u>	Pr(> t )			
(Intercept)	8.07e+00	1.01e+00	7.96	7.1e-11			
Speed >80% - 28day	-1.93e-05	4.30e-06	-4.50	3.3e-05			
Speed >80% - 56day	3.43e-05	7.24e-06	4.73	1.5e-05			
Previous Injury	3.04e-01	1.05e-01	2.91	0.0051			
Peak Nordic Force (N)	7.31e-03	1.50e-03	4.86	9.2e-06			
Time to Peak Angular Velocity	-2.12e-02	6.85e-03	-3.10	0.0030			
Time to 60deg/s Angular Velocity	2.35e-02	8.63e-03	2.73	0.0084			
Max Speed (m/s)	3.63e-01	8.66e-02	4.19	9.5e-05			
Nordic Force / BW (N/KG)	-7.45e-01	1.61e-01	-4.62	2.2e-05			
Age	-2.28e-02	1.43e-02	-1.59	0.1168			
Residual standard error: 1.11 on 58 degrees of freedom. Multiple R-squared: 0.572, Adjusted R-squared:							
0.506. F-Statistic: 8.62 on 9 and 58DF, p-value: 4.56e-08							

	Df	<u>Sum Sq</u>	<b>F-value</b>	<u>Pr(&gt;F)</u>
(Intercept)	1	78.0	63.37	7.1e-11
Speed >80% - 28day	1	24.9	20.24	3.3e-05
Speed >80% - 56day	1	27.6	22.42	1.5e-05
Previous Injury	1	10.4	8.46	0.0051
Peak Nordic Force (N)	1	29.1	23.64	9.2e-06
Time to Peak Angular Velocity	1	11.8	9.59	0.0030
Time to 60deg/s Angular Velocity	1	9.2	7.44	0.0084
Max Speed (m/s)	1	21.6	17.58	9.5e-05
Nordic Force / BW (N/KG)	1	26.3	21.34	2.2e-05
Age	1	3.1	2.54	0.11678
Residuals	58	71.4		

Supplementary Table 2: Analysis of Variance Type III (ANOVA):