

Research Bank

Journal article

**Assessing isometric kicking force and post-match responses
using the Kicker test**

**Thomas, Rees J., Timmins, Ryan G., Tofari, Paul J., Williams,
Morgan D. and Opar, David A.**

This is an Accepted Manuscript version of the following article, accepted for publication in *Journal of Sports Sciences*.

Thomas, R. J., Timmins, R. G., Tofari, P. J., Williams, M. D. and Opar, D. A.. (2022). Assessing isometric kicking force and post-match responses using the Kicker test. *Journal of Sports Sciences*, 40(11), pp. 1275-1281.
<https://doi.org/10.1080/02640414.2022.2065772>.

It is deposited under the terms of the Creative Commons Attribution-NonCommercial-NoDerivatives License, which permits non-commercial re-use, distribution, and reproduction in any medium, provided the original work is properly cited, and is not altered, transformed, or built upon in any way.

1 **Manuscript Title:** Assessing isometric kicking force and post-match responses using the Kicker test

2

3 **All institutions/laboratories where the study was carried out:**

4 • Melbourne Victory Football Club, Aami Park, 60 Olympic Boulevard, Melbourne, Vic, 3000,
5 Australia.

6 • Australian Catholic University, School of Behavioural and Health Sciences. 115 Victoria Parade,
7 Melbourne, Vic, 3065, Australia.

8

9 **Authors**

10 Rees J Thomas ^{a, b, c}

11 Ryan G Timmins ^{b, d}

12 Paul J Tofari ^b

13 Morgan D Williams ^c

14 David A Opar ^{b, d}

15

16 **Institutional (including department) affiliations of each author:**

17 ^a Melbourne Victory Football Club, Melbourne, Vic, Australia

18 ^b School of Behavioural and Health Sciences, Australian Catholic University, Melbourne, Vic, Australia

19 ^c College of Health and Biomedicine, Victoria University, Melbourne, Vic, Australia

20 ^d Sports Performance, Recovery, Injury and New Technologies (SPRINT) Research Centre, Australian
21 Catholic University, Fitzroy, VIC, Australia.

22 ^e School of Health, Sport and Professional Practice, Faculty of Life Sciences and Education, University of
23 South Wales, Treforest, United Kingdom

24

25 **Corresponding Author**

26 Name: Rees J Thomas

27 Email: reesjthomas@outlook.com

28 **Address:** Australian Catholic University, School of Behavioural and Health Sciences. 115 Victoria

29 Parade, Melbourne, Vic, 3065, Australia.

30 **Phone:** (+61) 413465030

31

32 **Sources of outside support for research:** The ForceFrame was provided to the research team free of

33 charge by Vald Performance.

34

35 **Word count:** 3937

36

37

38

39

40

41

42

43

44

45

46

47

48

49

50

51

52

53
54
55
56
57
58
59
60
61
62
63
64
65
66
67
68
69
70
71
72
73
74
75
76
77
78

ABSTRACT

This study examined the inter-session reliability of force output from a novel isometric strength assessment protocol (the Kicker); and the Kicker's suitability to monitor soccer player's combined hip flexion and knee extension force capacity over 72-hours post-competitive matches. Reliability (Part-A) testing was completed over three sessions on 20 individuals participating in various sports at a recreational level or higher. Post-match strength response (Part-B) data were collected for 72 hours (h) after a game (24 h (+24), 48 h (+48) and 72 h (+72) post-match) in 17 male academy soccer players. After familiarisation, Kicker force for each limb showed high inter-session reliability (intraclass correlation coefficients (ICC) >0.95; typical error (TE) <14 Newtons (N) (coefficient of variation (CV) <6%); minimum detectable change at a 95% confidence interval (MDC95%) <40N). Across the 72 hour post-match period, Kicker force for each limb was suppressed compared to baseline (force loss range = -5.8% to -12.5%; effect sizes (Cohen's *d*) range = -0.26 to -0.43) at all time points. The Kicker assessment protocol measures combined isometric hip flexor and knee extensor force capacity with high inter-session reliability. The proof of concept, that the protocol can be used as a monitoring tool was evidenced by sustained suppression of baseline force capacity in both kicking limbs for 72 hours post soccer matches.

Keywords: muscle strength, measurement, muscle injury, quadricep

79 INTRODUCTION

80

81 Field sports that involve kicking, such as soccer, carry a risk of strain injury to the quadriceps, with the
82 rectus femoris most commonly afflicted.¹ A recent 16 year follow up study of professional adult soccer
83 players showed that although the frequency of quadricep strain injury (5.7% of all injuries) is less than
84 hamstring strain injury (17.4% of all injuries), quadricep strain injuries result in a longer time to return to
85 play (19.5 days in quadriceps versus 18 days in hamstrings) and an equally high recurrence rate (15.6% in
86 quadriceps versus 17.5% in hamstrings). As there is a high burden and recurrence rate of quadriceps strain
87 injury, the prevention of these injuries is of paramount importance for practitioners.¹ In addition, injury
88 data from more than 40 elite youth soccer academies in the United Kingdom showed the quadriceps to be
89 the most frequent site of muscle strain injury,^{2,3} which suggest this injury is of even greater prominence in
90 this cohort.

91

92 Kicking is the most common mechanism for rectus femoris strain injury in soccer⁴ and is also the primary
93 injury mechanism in 8-13% of all injuries in high-level male youth soccer.⁵ The kicking action involves a
94 combination of hip flexion and knee extension during the leg acceleration phase to ball contact, although
95 the extent of this varies depending on kick type.⁶ As these two actions are the primary functions of the
96 biarticular rectus femoris, it is unsurprising that the action of kicking and injury to the rectus femoris are
97 closely linked.⁴

98

99 Elite sport settings often include periodic maximal strength testing to identify fluctuations in this capacity
100 as a form of secondary injury prevention.⁷ This form of screening is increasingly incorporated to identify
101 acute reductions in maximal strength (e.g., 48-72 hours post-competition) which may indicate sub-clinical
102 signs of pathology and a potential increased risk of future injury to the assessed muscle.^{8,9} The test
103 outcomes can provide information that may guide secondary prevention strategies, such as training load
104 modification (e.g., volume of goal shooting or sprinting) until strength scores return to baseline.^{10,11} This

105 approach has been reported recently for the adductors and knee flexors in similar cohorts of elite youth
106 male soccer players.^{10,11}

107

108 To assist with these secondary injury prevention strategies, practitioners require reliable tests for easy and
109 reproducible assessment of muscle strength.¹⁰ Reliable force tests for the separate isolated actions of the
110 kick exist (i.e., knee extension using hand-held dynamometry (HHD) and isokinetic dynamometry¹² and
111 hip flexion using HHD¹³), however, these isolated actions do not replicate the unique combination of joint
112 actions during the kick (ball contact phase) that place a high demand on the biarticular rectus femoris.¹⁴
113 Furthermore, although isokinetic dynamometry remains the gold standard for strength testing of knee
114 extension force¹⁵, it is expensive and time consuming¹⁶. Additionally, the reliance on the skill and strength
115 of the tester when using HHD, counteracts the benefits of cost and time efficiency.¹⁷ As a result, studies
116 examining the force production of kicking is likely limited by the lack of an appropriate and feasible test
117 of this action. More research is required to understand the specific strength demands of the muscles
118 involved in kicking and their recovery following a match.

119

120 A simple and practical field-based strength test of combined hip flexion and knee extension is required to
121 examine kicking related function/strength. Due to the combination of those joint actions, this test will
122 likely provide a surrogate measure to monitor the status of rectus femoris. An appropriate test could be
123 incorporated as a serial monitoring tool to determine the temporal function of rectus femoris following
124 match-play. Therefore, the aims of this study were to: a) describe a novel test to assess isometric strength
125 during a task that closely resembles the action of a kick (referred to as the Kicker); b) determine the inter-
126 session reliability of Kicker force; and c) evaluate the effect of competitive match-play on Kicker force
127 for a subsequent 72 hour period in academy soccer players, given their elevated risk of quadriceps strain
128 injury.

129

130 **MATERIALS AND METHODS**

131
132 Thirty-seven participants were recruited for this study that consisted of two parts. Part A examined the
133 inter-session reliability of the Kicker test on 20 participants (13 male, 7 female) partaking in various
134 sports at a recreational level or higher (age: 27.4 ± 4.3 years; height: 175.2 ± 7.8 cm). For Part B, post-
135 match strength response data were collected on 17 male academy soccer players (age: 18.0 ± 0.8 y;
136 height: 181.6 ± 8.4 cm; weight: 70.9 ± 9.5 kg). Analysis was then completed on 16 data points at +24 and
137 14 data points at +48 for both preferred and non-preferred limbs, and 10 and 11 data points at +72 for the
138 preferred and non-preferred limbs respectively. All academy soccer players were contracted to one
139 professional sporting team at the time of assessment, of which there were two goal-keepers, five
140 defenders, six mid-fielders and four forwards. The decision was made to conduct Part A and B in
141 different cohorts for several reasons. Firstly, to assess inter-session reliability of measures, it was
142 imperative that all participants presented to the lab in a standardized condition. To disrupt the professional
143 academy coaches and players' schedules to ensure they were in a rested state was considered unnecessary
144 and therefore unethical. Secondly, it was expected that the recreational athletes would be less skilled at a
145 kicking action compared to the academy soccer players and, therefore, the inter-session error detected in
146 the recreational athletes would provide a conservative (or larger) indication of the error in the Kicker that
147 could be utilized for further interpretation in Part B. This approach also allowed for Part A to inform the
148 design of Part B, with Part A providing guidance around the need and extent for familiarization to the test
149 prior to conducting data collection in Part B.

150
151 Participants in both Part A and B had no significant lower limb injury (i.e., no injury that resulted in
152 greater than six weeks of convalesces until return to given sport) in the previous six months. Informed
153 consent (including guardian consent and minor assent for participants under 18 years of age) and
154 institutional ethics approval were obtained (ACU HREC: 2017-245H). Participants were informed of the
155 benefits and risks of the investigation prior to signing the institutionally approved informed consent
156 document to participate in the study.

157

158 Reliability testing was performed at the School of Behavioural and Health Sciences, Australian Catholic
159 University in Melbourne. Post-match strength response data were collected at the Melbourne Victory
160 Football Club training facilities. All testing was completed by the lead investigator, who is a
161 physiotherapist with six years of clinical experience.

162

163 The Kicker test involved participants standing on the ForceFrame Strength Testing System (Vald
164 Performance, Albion, Queensland, Australia) with their stance leg heel in contact with the device handle
165 and the kicking leg (dorsum of foot) in contact with the device load cell (Figure 1). Participants held onto
166 the device bars and started with their kicking leg in a neutral hip position (0 degrees). The bar height
167 remained the same for each participant at the maximum height. The load cell height was customized for
168 each participant to ensure adequate foot clearance and optimal foot contact. Following a verbal cue,
169 participants completed a warm-up comprising a 50% and 75% maximum effort. After a 30 second rest,
170 participants performed three consecutive maximum repetitions, pushing through the dorsum of their foot
171 for three to five seconds. Participants were verbally encouraged during the contraction to ensure
172 maximum effort with a consistent command of “Kick, Kick, Kick”. Participants then had a 10 second rest
173 and repeated the test. In total, three efforts were completed for each limb. Less than 5 minutes was
174 required to administer the Kicker per participant. The single highest force (N) measure from any of the
175 three trials individually for the preferred and non-preferred limbs was determined as Kicker force. This
176 testing protocol was identical for both Part A and Part B of this study.

177

178 *(Insert Figure 1 here)*

179

180 Reliability data were collected between November 2017 and February 2018. Participants completed
181 testing on the same day and at the same time of day, for three consecutive weeks (3 testing sessions in
182 total, spanning 14 days). Post-match strength data were collected over four consecutive weeks between

183 July and August 2018 with the first of the four weeks (i.e., three testing sessions) completed as a
184 familiarisation week. Data collected from players who did not play ≥ 60 minutes (determined from
185 publicly available data) in the previous weekend's match were not used for the corresponding week's
186 analysis. Testing was always conducted within the 60 minutes prior to the commencement of training
187 sessions to minimise the impact of any acute fatigue. Testing time points were chosen to capture the first
188 72 h after a game and to correspond with the club's typical weekly system of player monitoring. Testing
189 time points coincided with a recovery day $24 \text{ h} \pm 2 \text{ h}$ (+24) post-match, upper body gym session $48 \text{ h} \pm 2$
190 h (+48) post-match, and a main skills training sessions $72 \text{ h} \pm 2 \text{ h}$ (+72) post-match. As a result, testing
191 for a given week was concluded prior to the main skills training session for that week.

192

193 Data from the inter-session reliability testing were uploaded to the device manufacturers cloud-based
194 repository. Normal distribution of the data was assessed in JMP® Pro version 14.2
195 (SAS Institute Inc., Cary, NC, USA) using a Shapiro-Wilks test. Data was then exported into a
196 customized Microsoft Excel spreadsheet¹⁸ designed to assess inter-session reliability. Mean differences
197 (and associated 95% confidence intervals), effect sizes (Cohen's d), intraclass correlation coefficient (ICC
198 3,1),¹⁹ typical error (TE), and TE as a coefficient of variation (%CV) were calculated to assess the extent
199 of variation between the first to second, and the second to third testing sessions.¹⁹ Based on Weir,¹⁹ it was
200 determined that an ICC >0.90 was high, between 0.80 and 0.89 was moderate, and <0.79 was poor.¹⁹

201 Minimum detectable change at a 95% confidence interval (MDC95) was calculated as $\text{TE} \times 1.96 \times \sqrt{2}$.²⁰

202

203 Post-match strength data were analysed using RStudio (Version 1.1.463) running the R programming
204 language (Version 4.0.5, *Shake and Throw*, The R Foundation for Statistical Computing). A linear mixed
205 effect model was used with player ID incorporated as a random intercept, which assessed the difference
206 post-match, in Kicker force across three time points and each limb (fixed effects) using
207 the *lmerTest* package in R. Where significant effects were seen, post hoc analysis was performed using
208 estimated marginal means, with significance set at $p < 0.05$. The time points, +24, +48, +72, were chosen

209 as they represent time points explored in previous studies looking at recovery of both isometric knee
210 extension and flexion force in soccer and Australian Football athletes respectively.^{21, 22} Furthermore,
211 testing time points were chosen to capture the first 72 h after a game and to correspond with the club's
212 typical weekly system of player monitoring. A rolling baseline was adopted for this component of the
213 study. During familiarization the highest Kicker force was recorded across three sessions as the baseline
214 score. If Kicker force in a subsequent week was higher than the previously defined baseline, a new
215 baseline was defined as this higher score, accordingly. We recorded the highest value for each time point
216 (+24, +48, +72) where we measured kicker force across the 3 weeks. To determine the size of the
217 differences at each time point, and to account for the dependency of repeated measurements,
218 Cohen's d_z was calculated with 95% confidence interval were calculated. Using the *effectsize* package, the
219 t value from the linear mixed model was divided by the square root of the degrees of freedom error from
220 the same model and interpreted as *trivial*, <0.20; *small*, 0.20-0.49, *moderate*, 0.50-0.79, and *large*,
221 ≥ 0.80 .^{23,24}

222

223 RESULTS

224

225 Of the 20 participants in Part A, 17 reported their right leg as their preferred kicking leg. All data was
226 normally distributed. Kicker force scores (N) across the three sessions were: 253±69, 258±64, 265±62
227 and 253±59, 259±56, 263±60 for the preferred and non-preferred limbs respectively. The ICCs ranged
228 from 0.91-0.98 and %CVs were below 10.3% for all sessions (Table 1). Effect sizes (Cohen's d) ranged
229 from 0.07-0.10 for all sessions (Table 1). Minimal detectable change scores at a 95% confidence interval
230 were below 49.3 N for all sessions (Table 1).

231

232 *(Insert Table 1 here)*

233

234 Seventeen participants were tested over three weeks in Part B. Of the 17 participants, 16 reported their
235 right leg as their preferred kicking leg. Twenty one data points were excluded from the analysis due to
236 incomplete data (due to injury, absence from training, or <60 minutes game time) leaving a total of 81
237 data points included in the analysis. This includes a single participant for which all testing data was
238 excluded. Testing did not interfere with players' regular training schedule and no participants were
239 injured during testing of the Kicker or reported any soreness on the testing day or in subsequent days.

240

241 There was a main effect reported for both time ($p<0.001$) and limb ($p<0.01$), but no interaction effect ($p=$
242 0.52) was observed. Following match-play, Kicker force remained suppressed compared to baseline in
243 both limbs at all time points ($p<0.01$). Loss in force capacity were -10.7% at +24 ($p<0.01$; $d= -0.39$), -
244 12.5% at +48 ($p<0.01$; $d= -0.43$) and -5.8% at +72 ($p<0.01$; $d= -0.26$) for the preferred limb and -9.2% at
245 +24 ($p<0.01$; $d= -0.35$), -9.8% at +48 ($p<0.01$; $d= -0.34$) and -7.8% at +72 ($p<0.01$; $d= -0.33$) for the non-
246 preferred limb (see Table 2 & Figure 2).

247

248

249 *(Insert Table 2 here)*

250

251 *(Insert Figure 2 here)*

252

253 **DISCUSSION**

254

255 This is the first study to explore the reliability of a combined hip flexion and knee extension isometric
256 strength test (the Kicker), and to examine the recovery of Kicker force output for 72 hours post-match in
257 academy soccer athletes. The major findings of this study were: a) the force outputs obtained from the
258 Kicker protocol display high levels of inter-session reliability; b) compared to baseline data, Kicker force
259 was suppressed post-match in both limbs at 24, 48 and 72 hours post-match; and c) there was no evidence

260 that Kicker force had returned to baseline levels at (72 hours post-match) the time typically expected
261 sufficient for full recovery and, according to weekly tactical periodization models, when soccer players
262 are exposed to stimulating training intensities.

263
264 This study demonstrates that the Kicker is a reliable assessment to measure combined hip flexion and
265 knee extension force. Furthermore, measurement error tended to lessen following the initial exposure to
266 the Kicker protocol (TE reduced from 17.6 N to 9.5 N and 17.8 N to 13.6 N for the preferred and non-
267 preferred limbs, respectively). This infers that a learning effect may exist and familiarisation to the test
268 may be important prior to collecting data intended to be used for further analysis.

269
270 The Kicker's ICC of 0.91-0.98 compares well to the reliability of an isokinetic dynamometer-based
271 isometric test of knee extension (ICC 0.93-0.96).²⁵ The reliability of isometric knee extension measured
272 using HHD suggests that it is a repeatable test (ICC 0.92-0.99),^{26,27} while HHD measures of isometric hip
273 flexion (ICC 0.86) tend to be somewhat less stable.¹⁷ The isometric protocol of the Kicker compares
274 favourably to dynamometer-based testing procedures due to being an externally fixed test (which is
275 superior to HHD) that is simple and easy to use in practice (which is superior to isokinetic dynamometry).
276 Furthermore, being able to combine the assessment of knee extension and hip flexion lends itself to a
277 more functionally relevant and time efficient (<5 minutes per participant) assessment of kicking function,
278 as opposed to independent, isolated movements.

279
280 The results of the reliability component (Part A) of this study allowed for inferences to be made regarding
281 post-match responses (Part B) in relation to the smallest detectable change of the test. As the reliability
282 data indicated a reduction in error with additional testing sessions, the post-match response portion of the
283 current work included a week of familiarization to minimize the impact of a learning effect. Therefore,
284 the reliability data comparing session 2 to session 3 (CV% = 3.7 to 5.3; MDC95% = 26 to 38 N) should
285 be used to guide the interpretation of the post-match response study.

286
287 Kicker force suppression was observed at all post-match testing time points (-10.7% at +24, -12.5% at
288 +48 and -5.8% at +72 [$p < 0.01$; d range -0.26 to -0.43]) for the preferred limb (-9.2% at +24, -9.8% at
289 +48 and -7.8% at +72 [$p < 0.01$; d range -0.33 to -0.35]) and for the non-preferred limb. There were some
290 outlier responses observed at some time points that would affect the amount of change observed. There
291 didn't appear to be anything obvious (e.g. player motivation etc.) that could explain these outliers.
292 Suppressed force capacity has been reported previously. Draganidis and colleagues²⁸ found that isometric,
293 concentric and eccentric knee extension strength and peak torque all did not return to baseline by 60 hours
294 post a soccer match and Thomas and colleagues²¹ found that isometric knee extension did not return to
295 baseline by 72 hours post simulated match play. Additionally, a recent systematic review and meta-
296 analysis showed that muscle force capacity (hamstring muscle group) and other fatigue related markers
297 (e.g., creatine kinase levels) remained substantially impaired 72 hours following actual and simulated
298 soccer match play.³⁰ What was different to previous reports however, was that based on those findings
299 knee extension and flexion strength and peak torque was anticipated to be lowest at 12 to 24 hours post-
300 match.^{28,30} There was no clear pattern in the current profiles across the 72 hours of post-match testing.
301 Understanding the shape and timeframe for recovery of Kicker force following matches has important
302 implications for its potential utility in soccer academies.

303
304 Armed with this novel assessment protocol, clinicians may be able to identify those with continued
305 suppressed force capacity. This may be useful from a secondary injury prevention perspective as a test to
306 help guide secondary prevention for quadriceps strain injuries. For example, monitoring the post-match
307 response to determine meaningful deviations (based on the MDC95% of 26 to 38 N) in Kicker force
308 could be used to inform modifications to training (e.g., shooting, sprinting) in the 72 hours post-match, as
309 has been recently described for the hamstrings.¹¹

310

311 While the current study aimed to establish the reliability and potential utility of the Kicker test from a
312 secondary injury prevention perspective, it may also have further applications that can be explored in
313 future work. For example, during rehabilitation from rectus femoris strain injury, a graded reintroduction
314 of kicking loads that replicates the demands required for match play is crucial for a safe return to play.³²
315 Clinical guidelines for return to kicking activities have been detailed in the literature,³² but do not provide
316 criteria for progression with respect to hip flexion and knee extension force and the subsequent
317 progressions through the kicking program. Monitoring Kicker force may provide an objective tool and
318 valuable outcome measure for monitoring kicking progressions over time and could be incorporated
319 within clinical guidelines to inform rehabilitation and more specifically kicking progressions following
320 rectus femoris strain injury, however, more work is needed in this area.

321
322 The current study was used as a proof of concept and therefore has some limitations that need to be
323 considered in this context. First, an absence of testing beyond 72 hours meant that the time course for full
324 restoration of Kicker force could not be determined. A 72-hour window of data collection post-match play
325 was utilized based on similar previous literature that deemed this sufficient to observe full restoration³⁰
326 and was also considered in light of contemporary coaching practice (i.e., weekly tactical periodization
327 models widely used in soccer). Furthermore, the absence of external load monitoring (e.g., running
328 distance and speeds etc.) and most importantly the number and type of kicks in a match/training meant
329 that no associations could be made between the impact of external loads to post-match Kicker responses.
330 It cannot be precluded that individual athlete external loads as well as other factors including motivation
331 or some athlete's pre-clinical pathology would influence some individual data points. It also should be
332 acknowledged that Part B utilized a convenience sample and investigation with a larger number of
333 participants would increase our confidence in these findings. Finally, as previously, reliability of the
334 Kicker was established in a different cohort of older recreationally active participants and not the
335 academy soccer players who were used for the post-match response component of the study. Differences
336 between the two cohorts (i.e. age disparity, distribution of gender, type and level of sport exposure,

337 kicking skill) should be considered when interpreting results. It is likely that the academy soccer players
338 who produced greater force outputs are more skilled at the kicking action and therefore the error in the
339 Kicker reported in the recreational athletes would overestimate the error in a soccer playing cohort.

340

341 In conclusion, the Kicker provides reliable data for the assessment of combined isometric hip flexor and
342 knee extensor force in recreationally active or higher participants from various sports. Kicker force is still
343 suppressed 72 hours after match play in both the preferred and non-preferred limbs in academy soccer
344 players. The Kicker provides a reliable and clinically feasible test that can be used to monitor combined
345 hip flexion and knee extension strength. This information may, in future, be used in conjunction with
346 return to kicking programs to help guide return to play following kicking related injuries.

347

348 **PRACTICAL APPLICATIONS**

349

350 Practitioners require reliable tests for easy, timely and reproducible assessment of muscle strength.¹⁰
351 There has previously been no simple and practical field-based strength test that measures the unique
352 combination of joint actions (combined hip flexion and knee extension) during the kick. The Kicker is a
353 reliable, quick to implement (<5 minutes) and safe to use (during the competitive season) test that can be
354 used to measure combined hip flexion and knee extension force. This test will likely provide a surrogate
355 measure to monitor the status of rectus femoris, as the action of kicking and injury to the rectus femoris
356 are closely linked.⁴ A familiarization session is important when utilizing the Kicker test to minimize
357 systematic error caused by possible learning effects. After familiarization, practitioners may interpret
358 Kicker force changes that exceed the CV% of 5.3% as real. Objective data from such a test may be useful
359 for practitioners during the rehabilitation of rectus femoris injuries in sports that involve kicking to
360 provide guidance for kicking progressions.

361

362

363 **ACKNOWLEDGEMENTS**

364

365 The authors thank Melbourne Victory Football Club coaches and players for their co-operation and
366 participation in this study. This research did not receive any specific grant from funding agencies in the
367 public, commercial, or not-for-profit sectors. The ForceFrame was provided free of charge to the research
368 team by Vald Performance. The authors would also like to thank Richard Johnston for his assistance with
369 the statistical analysis conducted for this manuscript.

370

371 **DECLARATION OF INTEREST STATEMENT**

372

373

374 Dr David Opar is listed as a co-inventor on a patent filed for a field-testing device of eccentric hamstring
375 strength (PCT/AU2012/001041.2012). The patent was filed by Queensland University of Technology
376 (QUT) and Dr Opar has received revenue distributions from QUT based on revenue the university has
377 generated from his intellectual property.

378

379 Dr Opar is a minority shareholder in Vald Performance Pty Ltd, the company responsible for
380 commercialising the device. Vald Performance has also commercialised the device utilised in the current
381 manuscript.

382

383 Dr Opar has received research funding from Vald Performance, for work unrelated to the current
384 manuscript. Dr Opar is the Chair of the Vald Performance Research Committee, a role that is unpaid. Some
385 of Dr Opar's family members are minor shareholders and/or employees of Vald Performance.

386

387 Dr Morgan Williams is a member of the Vald Research Committee. Dr Morgan Williams has been
388 provided donations of equipment, and funds for travel and subsistence by Vald Performance to conduct

389 research unrelated to this project. Dr Morgan Williams has received payment for reports for Vald
390 Performance unrelated to this and any research study.

391

392 The ForceFrame was provided to the research team free of charge.

393

394

395

396

397

398

399

400

401

402

403

404

405

406

407

408

409

410

411

412

413

414

415 **REFERENCES**

- 416 1. Ekstrand J, Krutsch W, Spreco A, et al. Time before return to play for the most common injuries in
 417 professional football: A 16-year follow-up of the UEFA elite club injury study. *Br J Sports Med.*
 418 2020;54(7):421-426. doi:10.1136/bjsports-2019-100666.
- 419 2. Read PJ, Oliver JL, De Ste Croix MBA, et al. An audit of injuries in six English professional
 420 soccer academies. *J Sports Sci.* 2018;36(13):1542–1548. doi.org/10.1080/02640414.2017.1402535
- 421 3. Cloke D, Moore O, Shab T, et al. Thigh muscle injuries in youth soccer: predictors of
 422 recovery. *Am J Sport Med.* 2012;40(2):433–439. doi: 10.1177/0363546511428800
- 423 4. Woods C, Hawkins RD, Hulse M, et al. The Football Association Medical Research Programme:
 424 an audit of injuries in professional football— analysis of preseason injuries. *Br J Sports Med.*
 425 2002;36:436–441. PubMed doi:10.1136/bjism.36.6.436.
- 426 5. Jones S, Almousa S, Gibb A, et al. Injury incidence prevalence and severity in high-level male
 427 youth football: a systematic review. *Sports Med.* 2019;49(12):1879-1899. doi 10.1007/s40279-
 428 019-01169-8
- 429 6. Brophy RH, Backus SI, Pansy BS, et al. Lower extremity muscle activation and alignment during
 430 the soccer instep and side-foot kicks. 2007. *J Orthop Sports Phys Ther.* 2007;37:260–268. doi:
 431 10.2519/jospt.2007.2255.
- 432 7. Ryan S, Kempton T, Pacecca E, et al. Measurement properties of an adductor strength assessment
 433 system in professional Australian footballers. *Int J Sports Physiol Perform.* 2019;14(2):256-259.
 434 doi: 10.1123/ijsp.2018-0264.
- 435 8. Crow JF, Pearce A, Veale, JP, et al. Hip adductor muscle strength is reduced preceding and during
 436 the onset of groin pain in elite junior Australian football players. *J Sci Med Sport.* 2009;13(2):202-
 437 204. doi: 10.1016/j.jsams.2009.03.007.
- 438 9. Thorborg K, Reiman, MP, Weir A, et al. Clinical examination, diagnostic imaging, and testing of
 439 athletes with groin pain: an evidence-based approach to effective management. *J*
 440 *Orthop Sports Phys Ther.* 2018;48(4):239-249. doi: 10.2519/jospt.2018.7850.

- 441 10. Wollin M, Thorborg K, Welvaert M, et al. In-season monitoring of hip and groin strength, health
442 and function in elite youth soccer: Implementing an early detection and management strategy over
443 two consecutive seasons. *J Sci Med Sport*. 2018;21(10):988-993. doi:
444 10.1016/j.jsams.2018.03.004.
- 445 11. Wollin M, Thorborg K, Drew M, et al. A novel hamstring strain injury prevention system: post-
446 match strength testing for secondary prevention in football [published ahead of print October 19,
447 2019]. *Br J Sports Med*. 2019. doi: 10.1136/bjsports-2019-100707.
- 448 12. Muff G, Dufour S, Meyer A, et al. Comparative assessment of knee extensor and flexor muscle
449 strength measured using a hand-held vs. isokinetic dynamometer. *J Phys Ther Sci*. 2016;28(9),
450 2445–2451. doi:10.1589/jpts.28.2445
- 451 13. Thorborg K, Petersen J, Magnusson SP, et al. Clinical assessment of hip strength using a hand-
452 held dynamometer is reliable. *Scand J Med Sci Sports*. 2010;20(3):493-501. doi: 10.1111/j.1600-
453 0838.2009.00958.x.
- 454 14. Mendiguchia J, Alentorn-Geli E, Idoate F, et al. Rectus femoris muscle injuries in football: a
455 clinically relevant review of mechanisms of injury, risk factors and preventive strategies. *Br J*
456 *Sports Med*. 2013;47(6), 359-366. doi:10.1136/bjsports-2012-091250.
- 457 15. Martin HJ, Yule V, Syddall HE, et al. Is hand-held dynamometry useful for the measurement of
458 quadriceps strength in older people? A comparison with the gold standard Biodex
459 dynamometry. *Gerontology*. 2006;52(3), 154-159. doi: 10.1159/000091824
- 460 16. Chamorro C, Armijo-Olivo S, De la Fuente C, et al. Absolute reliability and concurrent validity of
461 hand held dynamometry and isokinetic dynamometry in the hip, knee and ankle joint: systematic
462 review and meta-analysis. *Open Med*. 2017;12(1), 359-375. doi.org/10.1515/med-2017-0052
- 463 17. Kemp JL, Schache AG, Makdissi M, et al. Greater understanding of normal hip physical function
464 may guide clinicians in providing targeted rehabilitation programmes. *J Sci Med Sport*.
465 2013;16(4):292-6. doi: 10.1016/j.jsams.2012.11.887.

- 466 18. Hopkins WG, Marshall SW, Batterham AM, et al. Progressive statistics for studies in sports
467 medicine and exercise science. *Med Sci Sports Exerc.* 2009; 41:3–13. PubMed doi:10.1249/
468 MSS.0b013e31818cb278.
- 469 19. Weir JP. Quantifying test-retest reliability using the intraclass correlation coefficient and the SEM.
470 *J Strength Cond Res.* 2005;19(1):231–240. doi: 10.1519/15184.1.
- 471 20. Portney L, Watkins M. *Foundations of Clinical Research: Applications to Practice*, 3rd Ed.,
472 Philadelphia, PA: FA Davis, 2015.
- 473 21. Thomas K, Dent J, Howatson G, et al. Etiology and recovery of neuromuscular fatigue following
474 simulated soccer match-play. *Med Sci Sport Exer.* 2017; 49(5), 955-964
- 475 22. Charlton PC, Raysmith B, Wollin M, et al. Knee flexion strength is significantly reduced
476 following competition in semi-professional Australian Rules football athletes: Implications for
477 injury prevention programs. *Phys Ther Sport.* 2018; 31, 9-14. doi.org/10.1016/j.ptsp.2018.01.001
- 478 23. Cohen J. *Statistical Power Analysis for the Behavioral Sciences*. Hillsdale, NJ: Erlbaum, 1988.
- 479 24. Lakens, D. Calculating and reporting effect sizes to facilitate cumulative science: a practical
480 primer for t-tests and ANOVAs. *Front Psychol.* 2013; 4, 863.
481 <https://doi.org/10.3389/fpsyg.2013.00863>.
- 482 25. De Carvalho Froufe Andrade A, Caserotti P, De Carvalho C, et al.. Reliability of concentric,
483 eccentric and isometric knee extension and flexion when using the REV9000 isokinetic
484 dynamometer. *J Hum Kinet*, 2013;37(1), 47-53. doi: 10.2478/hukin-2013-0024.
- 485 26. Koblbauer IFH, Lambrecht Y, Van der Hulst, MLM, et al. Reliability of maximal isometric knee
486 strength testing with modified hand-held dynamometry in patients awaiting total knee arthroplasty:
487 Useful in research and individual patient settings? A reliability study. *BMC Musculoskelet Disord.*
488 2011;12, 249. doi: 10.1186/1471-2474-12-249.
- 489 27. Suzuki T. Reliability of measurements of knee extensor muscle strength using a pull-type hand-
490 held dynamometer. *J Phys Ther Sci.* 2015;27(3), 967-971. doi: 10.1589/jpts.27.967.

- 491 28. Draganidis D, Chatzinikolaou A, Avloniti A, et al. Recovery kinetics of knee flexor and extensor
492 strength after a football match. *PLoS One*. 2015; 10(6):e0133459. doi:
493 10.1371/journal.pone.0128072.
- 494 29. Thomas K, Dent J, Howatson G, et al. Etiology and recovery of neuromuscular fatigue following
495 simulated soccer match-play. *Med Sci Sport Exer*. 2017; 49(5), 955-964.
- 496 30. Silva JR, Rumpf MC, Hertzog M, et al. Acute and residual soccer match-related fatigue: A
497 systematic review and meta-analysis. *Sports Med*. 2018;48(3):539-583. doi: 10.1007/s40279-017-
498 0798-8.
- 499 31. Silva JR, Ascensão A, Marques F, et al. Neuromuscular function, hormone and redox status and
500 muscle damage of professional soccer players after a high-level competitive match. *Eur J Appl*
501 *Physiol*. 2013;113(9):2193–2201. doi: 10.1007/s00421-013-2633-8
- 502 32. Arundale A, Silvers S, Logerstedt D, et al. An interval kicking progression for return to soccer
503 following lower extremity injury. *Int J of Sports Phys Ther*. 2015;10(1), 114-127.
- 504 33. Brownstein CG, Dent JP, Parker P, et al. Etiology and recovery of neuromuscular fatigue
505 following competitive soccer match-play. *Front Physiol*, 2017;8, 831-845.
506 <https://doi.org/10.3389/fphys.2017.00831>
- 507
508
509
510
511
512
513
514
515
516

517 **Tables**

518

519 **Table 1:** Inter-session reliability of force data (N) for the Kicker test comparing session 1 to 2, and 2 to 3

520 respectively.

Test	Side	Mean difference (95% CI)	Cohen's d	ICC (95% CI)	TE (95% CI)	%CV (95% CI)	MDC95 (N)
2-1	Preferred Leg	5.2 (-6.46 to 16.9)	0.08	0.94 (0.85 to 0.97)	17.6 (13.4 to 25.7)	10.3 (7.7 to 15.3)	49
	Non- preferred Leg	6.0 (-5.8 to 17.8)	0.10	0.91 (0.80 to 0.97)	17.8 (13.6 to 26.1)	9.2 (6.9 to 13.8)	49
3-2	Preferred Leg	6.3 (-0.01 to 12.5)	0.10	0.98 (0.95 to 0.99)	9.5 (7.2 to 13.8)	3.7 (2.8 to 5.4)	26
	Non- preferred Leg	4.0 (-5.0 to 13.0)	0.07	0.95 (0.88 to 0.98)	13.6 (10.3 to 19.9)	5.3 (4.0 to 7.9)	38

521 ICC: intraclass correlation coefficient; CI: confidence interval; TE: typical error; %CV: typical

522 error as a coefficient of variation; MDC95: Minimum detectable change; N: Newtons.

523

524

525

526

527

528

529

530

531

532 **Table 2:** Within- group data and effect size (95%CI) of changes in Kicker force 24, 48 and 72 hours
 533 following competitive match play compared to baseline.

534

Time	Mean \pm SD (N)	P Value	Effect size estimate (95% CI)
Preferred Leg			
Baseline	343 \pm 39	-	-
+24 (n=16)	306 \pm 53	<0.01	-0.39 (-0.53 to -0.26)
+48 (n=14)	300 \pm 56	<0.01	-0.43 (-0.57 to -0.29)
+72 (n=10)	323 \pm 44	<0.01	-0.26 (-0.39 to -0.13)
Non-preferred Leg			
Baseline	351 \pm 43	-	-
+24 (n=16)	319 \pm 43	<0.01	-0.35 (-0.48 to -0.21)
+48 (n=14)	317 \pm 46	<0.01	-0.34 (-0.47 to -0.20)
+72 (n=11)	324 \pm 39	<0.01	-0.33 (-0.46 to -0.19)

535 SD: standard deviation; CI: confidence interval; L: left; R: right; N: Newtons

536

537

538

539

540

541

542

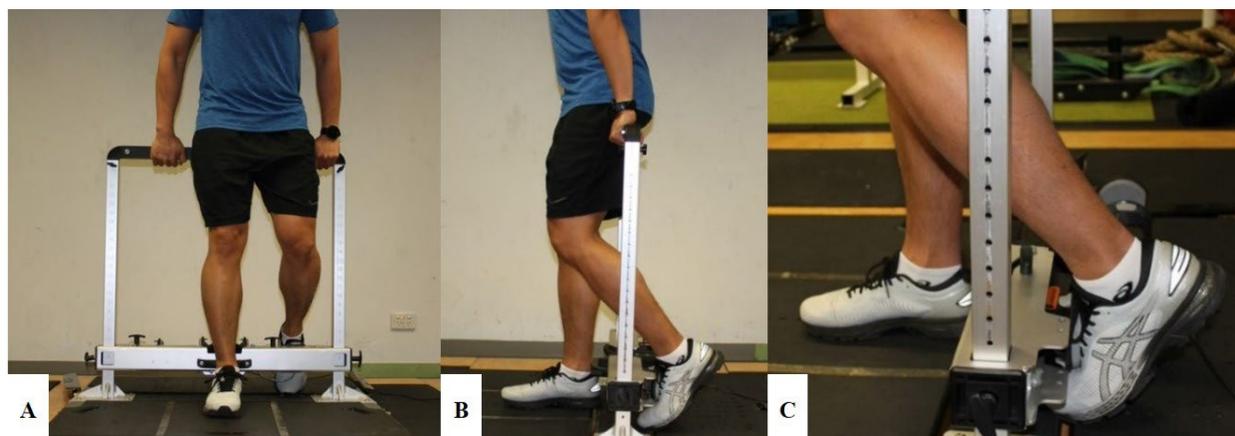
543

544

545

546 **Figure 1**

547



548

549

550

551

552

553

554

555

556

557

558

559

560

561

562

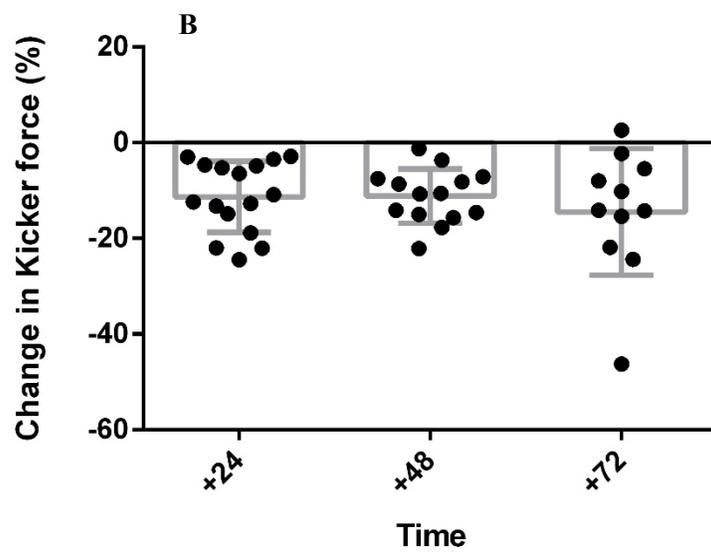
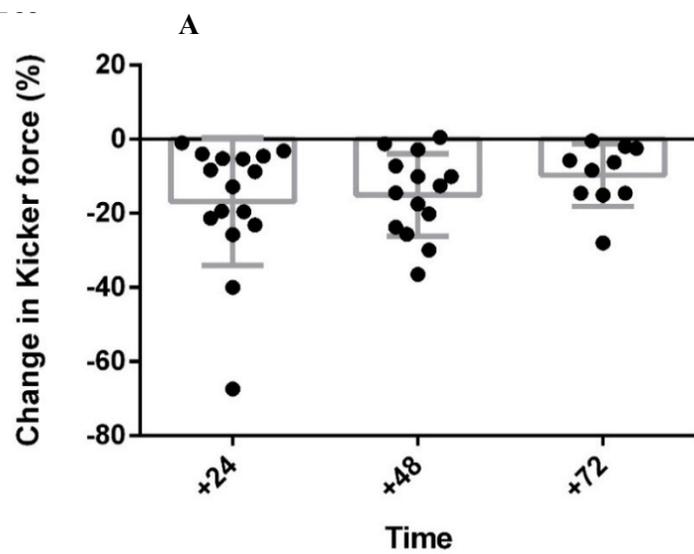
563

564

565

566 Figure 2

567



592 **Figure Captions**

593

594 **Figure 1:** Kicker setup: A) Front on and B) side on view of participant standing on ForceFrame, holding
595 onto the bar, with buttocks in contact with bar. Back of stance leg in contact with crossbar handle and
596 kicking leg in contact with load cell. C) Dorsum of foot (participants defined best contact point) in contact
597 with device load cell.

598

599 **Figure 2:** Percentage change in Kicker force, compared to baseline, for the: A) Preferred leg and B) Non-
600 preferred leg 24, 48 and 72 hours following a competitive soccer match.

601